#### BREAST



# Virtual clinical trial to compare cancer detection using combinations of 2D mammography, digital breast tomosynthesis and synthetic 2D imaging

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## Abstract

**Objectives** This study was designed to compare the detection of subtle lesions (calcification clusters or masses) when using the combination of digital breast tomosynthesis (DBT) and synthetic mammography (SM) with digital mammography (DM) alone or combined with DBT.

**Methods** A set of 166 cases without cancer was acquired on a DBT mammography system. Realistic subtle calcification clusters and masses in the DM images and DBT planes were digitally inserted into 104 of the acquired cases. Three study arms were created: DM alone, DM with DBT and SM with DBT. Five mammographic readers located the centre of any lesion within the images that should be recalled for further investigation and graded their suspiciousness. A JAFROC figure of merit (FoM) and lesion detection fraction (LDF) were calculated for each study arm. The visibility of the lesions in the DBT images was compared with SM and DM images.

**Results** For calcification clusters, there were no significant differences (p > 0.075) in FoM or LDF. For masses, the FoM and LDF were significantly improved in the arms using DBT compared to DM alone (p < 0.001). On average, both calcification clusters and masses were more visible on DBT than on DM and SM images.

**Conclusions** This study demonstrated that masses were detected better with DBT than with DM alone and there was no significant difference (p = 0.075) in LDF between DM&DBT and SM&DBT for calcifications clusters. Our results support previous studies that it may be acceptable to not acquire digital mammography alongside tomosynthesis for

subtle calcification clusters and ill-defined masses.

#### **Key Points**

- The detection of masses was significantly better using DBT than with digital mammography alone.
- The detection of calcification clusters was not significantly different between digital mammography and synthetic 2D images combined with tomosynthesis.
- Our results support previous studies that it may be acceptable to not acquire digital mammography alongside tomosynthesis for subtle calcification clusters and ill-defined masses for the imaging technology used.

#### Keywords Screening · Mammography · Cancer

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Abbreviations				
DF	Degrees of freedom			
DM	Digital mammography			
FoM	Figure of merit			
FRF	False recall fraction			
JAFROC	Jackknife alternative free-response receiver oper-			
	ating characteristics			
LDF	Lesion detection fraction			
MGD	Mean glandular dose			
SM	Synthetic 2D images			

## Introduction

Several clinical trials have investigated if synthetic 2D image (SM) (created from the tomosynthesis images) can be used instead of acquiring 2D digital mammograms (DM) in combination with digital breast tomosynthesis (DBT) [1-7]. This would reduce the radiation dose received by women, but could affect cancer detection rate. The SM images are likely to be technically inferior due to extra geometric blurring during the continuous acquisition of projection images under different angles or due to electronic noise accumulating from multiple low-dose projection images [8]. Clinical trials have not found any statistical difference in cancer detection between using DM or SM combined with DBT [9-11]. However, such clinical trials have potential issues with achieving sufficient numbers of subtle cases and can have many confounding factors, such as different women in the study arms, different imaging systems and image readers, which may result in a different distribution of lesions in the study arms. It may be that only relatively large differences could be found to be statistically significant, even with large numbers of women. Another approach is to use validated virtual clinical trials (VCTs) that include the insertion of simulated lesions into images (either mammograms or images of breast phantoms) which are then interpreted by experienced mammography readers. Such studies reduce the number of variables and can find statistically significant and valuable results over a reduced time-frame and allow easier stratification by lesion type [12].

This study was designed to assess the performance of the combination of DBT and SM on the detection of realistic subtle lesions (calcification clusters and masses) compared to that of DM alone or combined with DBT. The use of subtle lesions improves the sensitivity of the study, which enables the detection of smaller differences than would be possible in all but the largest standard clinical trials.

## Materials and methods

Ethical approval was obtained for this study as part of the OPTIMAM project as well as local ethical committee approval for the retrospective collection of the cases at the test site.

#### Image collection

The images used in this study were collected from a Siemens Inspiration mammography system (Siemens Healthcare) at UZ Leuven (UZL), Belgium.

A set of 300 cases recalled for a suspected cancer in one breast with images acquired between June 2017 and October 2017 was identified. The images of the contralateral breast were used for the study. An expert radiologist, with 27 years of mammography reading experience, assessed the images to confirm that there were no features of either malignant or benign lesions. Images with memorable features such as distinctive calcifications or clips were also excluded from the dataset. A dataset of 166 cases, using a single view (either cranio-caudal or medio-lateral oblique), was randomly selected for the study and included breasts of all BI-RADS density categories. From follow-up, 160 of the cases had no new cancer diagnosis in the breast used within 2 years, while 6 cases did not have any follow-up.

## Insertion of calcification clusters and masses in images

Models of calcification clusters were created from images of calcifications segmented from micro-CT images of biopsy samples [13]. Voxel models of simulated round masses with illdefined borders were created using a fractal growth method known as diffusion limited aggregation, where they were shown to be indistinguishable from real masses [14]. The mass diameter ranged from 4 to 8 mm. The insertion sites within the breasts were randomly chosen and covered the complete breast volume. There were limitations applied such as insertions were more than 5 mm from the skin line and at a height of between a fifth and four-fifths of the compressed breast thickness.

A breast density map was acquired for each image using Volpara software (version 1.5.4, Volpara Health Technologies Ltd.) [15]. The average density at the location of lesion insertion was estimated. This ensured that the lesion was inserted with the correct contrast. The simulated lesions were inserted into the unprocessed DM and DBT projection images using validated methods [16]. Registration of the DM images and the central DBT projection images was undertaken, to insert the lesions in the corresponding locations in the SM and DM images. The DBT series, with 1 mm separation between the planes, and synthetic 2D images were reconstructed from these projection images. Examples of the appearance of a calcification cluster and mass in DM, DBT and SM images are shown in Figs. 1 and



Fig. 1 Extracted calcification cluster used in this study: DM (left), one DBT plane (middle), synthetic 2D (right)

2. Only images that were considered realistic by an expert radiologist were included in the study.

## **Reader study**

The study dataset comprised:

- 62 normal cases
- 64 cases with simulated calcification clusters with a total of 80 calcification clusters inserted
- 40 cases, each with one simulated ill-defined mass

A reader study was conducted using the full study dataset based on imaging modality combinations:

- Arm D: DM only
- Arm D&T: DM and DBT displayed simultaneously
- Arm S&T: SM and DBT displayed simultaneously.

The 166 cases in the three study arms were then randomly arranged into 18 sets, such that each set contained cases from the three study arms. All images were viewed by five readers experienced in reporting screening mammograms and DBT images acquired on Siemens systems. The readers had between 1 and 21 years' experience in reading breast images and between 1 and 5 years' experience in reading DBT cases and each reading over 3500 screening mammography cases annually. Readers were recruited from St George's Hospital, London and UZL, Leuven. The cases were shown to the readers using the MedXViewer software [17] on a workstation with two 5 megapixel reporting monitors (Barco MDMG (Barco NV)).

The readers viewed the image sets consecutively, but in a different order from the other readers. To reduce memory effects, the MedXViewer software enforced a minimum of 14 days between viewing images of the same case in a different study arm. Readers could use panning and magnification facilities on the MedXViewer software. Initially, the images were scaled to fit the monitor and the reader could scroll through the DBT stack of individual planes.

The task of the readers was to mark the centre of any lesion within the images that should be recalled for further investigation. The readers were not made aware of the design of the study. Readers marked the lesion in the DBT plane with the highest lesion conspicuity. The readers had a choice of two images to mark in study arms D&T and S&T; in those cases, they were asked to mark the lesion location on the image in which the lesion was most clearly seen. Following a mark, the reader was asked:

- Question 1:What type of lesion is this? Calcification cluster; mass; calcification cluster + mass
- Question 2:What is your level of confidence that this lesion should be recalled? 1–100%
- Question 3:How visible is the lesion in the other image? Not visible; less visible; similar visibility

Fig. 2 Extracted ill-defined mass used in this study: DM (left), one DBT plane (middle), synthetic 2D (right)



The coordinates of the marks made by the readers and their answers to the questions were automatically saved by the MedXViewer software.

## Data analysis of reader study

The region of interest (ROI) for each lesion was defined as the margin of the inserted lesion. A mark was classed as a lesion localisation when it was inside a ROI and the lesion type matched the response to question 1. If a mark was not within a ROI or the lesion type was misidentified, it was classified as a non-lesion localisation. JAFROC-4.2 software (www. devchakraborty.com) [18] was used to evaluate the marks. The calculation of jackknife alternative free-response receiver operating curves (JAFROC) was undertaken for random readers and random cases; i.e. the readers and cases were thought to be representative of their respective populations. A global *F*-test using the null hypothesis that all the arms are equal was included in the JAFROC testing. The equally weighted JAFROC figure of merit (FoM) was used to estimate the overall effectiveness of each imaging modality. The statistical difference between the FoMs was undertaken using the Dorfman-Berbaum-Metz analysis of variance [19].

The lesion detection fraction (LDF) was computed for calcification clusters and masses separately from the lesion localisation fraction. The false recall fraction (FRF) was computed from the non-localisation fraction of marks made in cases that did not have an inserted lesion.

The results for question 3 were collated for the D&T and S&T arms. The 3-point score of the comparative visibility of the lesions between 2D and DBT was converted to a 5-point scale of 'Not visible in DBT', 'Less visible in DBT', 'Similar', 'More visible in DBT' and 'Only visible in DBT'. The conversion depended on the score and if the 2D (DM or SM) or DBT image was marked.

## Results

The alternative free-response receiver operating characteristic (AFROC) curves for the combined scores of the readers for calcification clusters and masses are shown in Fig. 3a and b, while Fig. 3c and d show their equivalent JAFROC FoM. The global *F*-test of the FoM produced *F*-values equal to 1.97 (degrees of freedom (DF) of 2 and 79) and 30.7 (DF of 2 and 39) for the calcification clusters and masses respectively. The resultant *p* values between the study arms were 0.18 and < 0.0001 for calcification clusters and masses respectively; i.e. the difference was only statistically significant for the masses. Figure 3e and f show the JAFROC FoM for each reader; although the absolute values vary between readers, broadly they produce the same comparison, with the exception of

reader 1 who found arms D and D&T significantly better than S&T ( $p \le 0.0008$ ).

The LDFs are shown in Fig. 4. The highest LDFs were 43% (D&T) and 59% (S&T) for calcification clusters and masses respectively. Sixty-eight of the 80 clusters were marked by at least one reader and 37 of 40 masses in at least one of the study arms. Only one of 80 calcification clusters and one of 40 masses were marked by all readers in the three study arms. This indicates that the lesions included in the study were very subtle. The percentage differences between the JAFROC FoMs and LDFs are shown in Tables 1 and 2. No significant differences were found for the detection of calcification clusters. The detection of masses in DM images alone was significantly worse than either of the arms which included DBT.

Figure 5 shows the FRF for non-lesion localisation marks of calcification clusters and masses in the normal images. The only significant differences shown in Tables 1 and 2 were that the D arm has a significantly lower FRF for masses than the other two study arms (p < 0.0012).

Figure 6 shows the visibility of the lesions in the DM and SM images compared to the DBT images. For calcification clusters, the most common selected option was that the clusters in DM and SM images were similar in visibility to the DBT image. The next most popular option was that the clusters were more easily seen in the DBT. Calcifications clusters were marked as only visible on DM in 12/80 clusters, and marked as only visible on DBT in 6/80 clusters. For masses, there was a clear preference for DBT over DM and SM images, and there were no masses only seen in DM or SM images but 18/40 cases where the mass was only visible in DBT.

## Discussion

This VCT was designed to compare detection of subtle lesions between different combinations of mammographic imaging techniques. All of the lesions used in this study were visible in at least one of the image types but not all of the lesions were recalled as they were often on the cusp of the recall/not recall decision. By concentrating on subtle cases, this VCT avoids the need for very large numbers of cases to demonstrate the difference in cancer detection rate using combinations of DM, SM and DBT. This study has shown that the detection of masses was significantly improved with DBT over DM alone. In addition, lesion detection with SM combined with DBT was not significantly lower than that with DM and DBT for calcification clusters.

We used realistic small masses that were difficult to detect on DM imaging. In common with other publications [6, 20, 21], there was a clear difference in the detection of masses between DM alone and when DBT was included. The visibility of masses is clearer with DBT due to the reduction in the Fig. 3 Reader-averaged AFROC curves for (a) calcification clusters and (b) masses. Solid and dashed lines = measured data. dotted lines = straight line extension to (1,1) defining the area under the curve which is included in the FoM. c, d JAFROC FoMs averaged for all readers for each arm combination. e, f JAFROC FoMs for each reader and arm combination. Error bars indicate 95% confidence intervals









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Difference between arms	FoM	LDF	FRF
D&T – D	0.9% (0.84)	3.6% (0.72)	30% (0.61)
S&T – D	- 7.1% (0.13)	- 15% (0.15)	20% (0.73)
S&T – D&T	- 8.0% (0.09)	- 18% (0.075)	- 7.7% (0.86)
	Difference between arms D&T – D S&T – D S&T – D&T	Difference between arms FoM   D&T - D 0.9% (0.84)   S&T - D - 7.1% (0.13)   S&T - D&T - 8.0% (0.09)	Difference between arms FoM LDF   D&T - D 0.9% (0.84) 3.6% (0.72)   S&T - D - 7.1% (0.13) - 15% (0.15)   S&T - D&T - 8.0% (0.09) - 18% (0.075)

overlap of the background breast parenchyma. The use of DBT greatly increased the detection of masses and in this case the combination of DM imaging with DBT did not improve mass detection compared with DBT with SM.

The use of imaging technology will not only result in the detection of malignant masses but also allow the detection of benign masses that can appear similar to malignant masses. This study was focussed on testing the detection of small ill-defined masses, rather than distinguishing between malignant and benign lesions. A significant increase ( $p \le 0.0012$ ) in the FRF was found for the two study arms including DBT images compared to digital mammography alone. A clinical study would be required to evaluate the overall impact of DBT on detection of extra cancers and over-investigation.

Four readers found no difference in the detection of calcification clusters when SM images were used instead of DM images alongside DBT, while one reader found that including DM images significantly improved detection ( $p \le 0.0008$ ). A larger study is needed to demonstrate if the average reduction in detection becomes significant for these subtle and small calcification clusters. Most malignant calcification clusters can be in situ or invasive cancers but more often represent ductal carcinoma in situ (DCIS). The detection of low-grade DCIS has been associated with overtreatment. It has been shown that the use of DBT can increase this over-diagnosis [22].

Consistent with other works, we found that the detection of lesions increased with the use of DBT compared to DM alone due to the extra masses detected, while there was little or no difference in the detection of calcification cluster rates [6, 21, 23, 24]. Houssami [9] reviewed five studies [2–7] comparing DBT&DM and DBT&SM and concluded that in population screening cancer detection rates do not differ between DBT&DM (range, 5.45–8.5/1000 screens) and DBT&SM (range, 5.03–8.8/1000 screens). She found that there was a wide range in recall rates between the studies but only small differences were found between the modalities. Houssami concluded that it was safe to transition to only acquiring the DBT images without the DM images. However, on close examination of the papers, four of the five studies showed a non-significant decrease in cancer detection rate for SM&DBT vs DM&DBT. She also reported on studies using enhanced data sets [25–27], and three of the studies showed non-significant lower scores in the comparison of SM&DBT against 2D&DBT. Martín et al [10] showed a non-significant decrease of 6.7% in cancer detection when SM replaced DM imaging. This indicates that small differences in lesion detection using SM rather than DM with DBT are difficult to prove with a clinical trial. Our study only used subtle cases and has also shown a non-significant drop in lesion detection for calcification clusters.

Our study included a comparison of the visibility of the calcification clusters between DBT and DM images. There is evidence that the smallest calcifications within a cluster that are visible on DM may not be visible in DBT or SM images [28, 29]. The SM images are constructed from DBT and suspicious regions may be enhanced in the SM image compared with DM image. Calcification clusters typically contain a range of calcification sizes and even if some calcifications are not visible within a cluster using DBT, the larger calcifications may be enhanced and aid detection [30]. Our work showed that the visibility of calcification clusters was considered similar between DBT and DM images, but also that some subtle clusters were more visible in DBT than DM images. This is consistent with Korhonen et al [31]. Many publications [9, 32] support the idea of not acquiring a DM image in conjunction with DBT images, which has the advantage of reducing the radiation dose of the examination. However, there is potentially a loss in detection of sub-types of lesions, e.g. calcification clusters [3]; the results of our study show that this may not be the case for the technology used here.

The use of VCTs can aid faster investigations into specific areas of interest and more valid comparison between different

**Table. 2**Masses: the percentagedifference in JAFROC-weightedFoM, LDF and FRF relative to thesecond arm in the first column.p values are given in parentheses

Difference between arms	FoM	LDF	FRF
D&T – D	35% (< 0.0001*)	210% (< 0.0001*)	54.2% (0.0005*)
S&T – D	39% (< 0.0001*)	240% (< 0.0001*)	50% (0.0012*)
S&T – D&T	3.0% (0.46)	6.3% (0.43)	- 2.7% (0.77)

\*Significant difference p < 0.05

Fig. 5 False recall fraction (FRF) for all non-lesion localisation marks in cases without lesions. **a** Calcification clusters. **b** Masses. Error bars indicate 95% confidence intervals



imaging modalities, and allow deeper investigation into the nuances of image interpretation than conventional clinical trials. However, a VCT should not be considered directly comparable with a clinical trial, rather as adding sophisticated information that aids interpretation of clinical trials. Perception and interpretation are both important initial steps in the assessment of a mammogram/DBT, which may be modified by comparison with priors and the opposite breast. As we have used one breast and one view with no priors, then we only examined this first



Fig. 6 Total number of marks of classification of visibility of lesions in 2D images (DM or SM) compared to DBT in arms D&T and S&T. a Calcification clusters. b Masses

stage. This study examines the detection of lesions and did not include benign lesions to examine the discriminatory power of the different study arms. Although the lesions were simulated, the process of simulating and inserting these lesions has been validated [16]. In addition, all of the lesions were checked for realism by an expert radiologist. This study is limited to one imaging system, as the appearance of the lesion may have been different with other systems, due to the scan angle, the DBT reconstruction algorithm [33], 2D post-processing [34, 35] and SM algorithm.

This study has examined the effect of using different types of mammographic images on lesion detection. No significant differences in the detection of calcification clusters were found between the arms of the study, but there was significantly better detection of masses when DBT was included. This work indicates that the acquisition of a DM image alongside a DBT image may not be necessary. Using a study with only subtle lesions, our results support the results of many previous studies that it may be acceptable to not acquire digital mammography alongside tomosynthesis for subtle calcification clusters and ill-defined masses.

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#### **Declarations**

**Guarantor** The scientific guarantor of this publication is Prof. Kenneth C. Young (ken.young@nhs.net).

**Conflict of interest** The authors of this manuscript declare relationships with the following companies:

Chantal Van Ongeval: research and travel agreements with Siemens Healthineers; research agreement with GE Healthcare.

Lesley Cockmartin's lab has research agreements with Siemens Healthineers and GE Healthcare.

Matthew Wallis: This research was supported by the NIHR Cambridge Biomedical Research Centre (BRC-1215-20014). The views expressed are those of the authors and not necessarily those of the NIHR or the Department of Health and Social Care.

**Statistics and biometry** Two of the authors (LMW, AM) have significant statistical expertise for this type of study.

**Informed consent** Written informed consent was waived by the Institutional Review Board.

Ethical approval Institutional Review Board approval was obtained.

**Study subjects or cohorts overlap** Five cases were used in a previous publication (https://www.spiedigitallibrary.org/conference-proceedings-of-spie/10952/109520U/An-observer-study-to-assess-the-detection-of-calcification-clusters/10.1117/12.2506895.full). In those cases, either the images used were a different view or a different lesion was inserted.

#### Methodology

- not applicable (prospective/retrospective)
- experimental
- multicentre study

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