Annotation-Efficient Deep Semi-Supervised Learning for Automatic Knee Osteoarthritis Severity Diagnosis from Plain Radiographs

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1 Introduction

Osteoarthritis (OA) is a worldwide disease that occurs in joints causing irreversible damage to cartilage and other joint tissues. The knee is particularly vulnerable to OA, and millions of people, regardless of gender, geographical location, and race, suffer from knee OA. When the disease reaches the late stages, patients have to undergo a total knee replacement (TKR) surgery to avoid disability. For society, direct and indirect costs of OA are notably high, and for instance, OA is one of the five most expensive healthcare expenditures in Europe [1]. In the United States, the burden of knee OA is also huge, and TKR surgeries annually cost over 10 billion dollars [2]. If knee OA could be detected at an early stage, its progression might be slowed down, thereby yielding significant benefits at personal and societal levels [3].

Radiographs, affordable and widely available in primary care, are sufficiently informative for knee OA severity diagnosis. However, the process of visual assessment of radiographs is rather tedious, and as a result, various Deep Learning (DL) based methods for automatic diagnosis of knee OA severity have recently been developed [4–6]. The primary drawback of these methods is their dependency on large amounts of annotations, which are expensive in terms of cost and time to collect.

In this paper, we introduce *Semixup*, a novel Semi-Supervised Learning (SSL) method, which we apply for automatic diagnosis of the knee OA severity in an annotation-efficient manner. This extended abstract is a short version of [7].

2 Method

2.1 Data

Our datasets were from the Osteoarthritis Initiative (OAI) and the Multicenter Osteoarthritis Study (MOST) patient cohorts. While OAI data were used for training and validation, MOST data were used for an independent testing. Bilateral posterior-anterior knee radiographs in those datasets were acquired in fixed flexion using Synaflexer® positioning frame and 10° beam angle. All available radiographs from all the follow-ups in the OAI were utilized. In the MOST dataset, we applied similar strategy, but excluded the images acquired with 5° or 15° beam angle as well as the ones without the Osteoarthritis Research Society International (OARSI) scores. We used the Kellgren Lawrence (KL) grading [8] as a reference standard to assess the severity of knee OA. The KL system classifies OA in 5 levels, where 0 indicates no signs of OA, 1 – doubtful OA, 2 – early OA, 3 – moderate OA, and 4 –

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end stage OA. After the data selection phase, we obtained 39,902 and 3,445 knee images for training and independent evaluation phases, respectively.

For training and model selection, we formed 4 settings of annotation data: 50, 100, 500, and 1000 samples with annotation per KL grade, each of which has 6 unannotated data settings: $1 \times, 2 \times, ...$, $6 \times$ more samples without annotation. Thus, in total, we had 24 data settings for SSL methods. In addition, we gathered all annotated data in the OAI to form a large data setting for training a SL model.

2.2 Siamese Architecture

We designed a Siamese DL architecture for all SL and SSL methods [7]. The main component in the model is 3×3 convolutional blocks of a 3×3 convolutional layer, an instance normalization, and a LeakyRELU activation. The network has 4 subsampling layers separating groups of 3×3 convolutional blocks, and in the bottleneck, it produces a feature map of 16×16 for a given 128×128 input image in each branch of the model. Each of the feature maps is compressed into 1×1 feature by a pooling layer. Finally, we concatenate the features from each of the branches and use a fully connected layer to predict the KL grades.

To extract the left and right knee sides for our Siamese network, we closely followed [6], except that we performed a tighter crop with the size $110mm \times 110mm$ instead of $130mm \times 130mm$ and used a mean of 0.5 and a standard deviation of 0.5 instead of extracting them from OAI data. As a result, we obtained pairs of 128×128 -pixel images (0.37mm pixel spacing).

2.3 Semixup

The core idea of our method is to enforce continuous predictions within and out of the data manifold \mathcal{M} . As such, explicitly enforce the smoothness of predictions within the data manifold $\mathbb{E}_x ||J_{\mathcal{M}}||_F^2$, where $J_{\mathcal{M}}$ denotes the Jacobian along the data manifold \mathcal{M} and $|| \cdot ||_F$ is the Frobenius norm. To achieve this, we use *consistency regularization*, which widely used in the SSL domain [9], and thus minimize:

$$\mathbb{E}_{x \sim p(x)} \mathbb{E}_{T, T' \sim p(\tau)} \left\| f_{\theta}(Tx) - f_{\theta}(T'x) \right\|_{2}^{2}, \tag{1}$$

where f_{θ} is our model with learnable parameters θ , p(x) is the distribution of annotated and unannotated data, and $p(\tau)$ is the distribution of stochastic transformations.

To generate the out-of-manifold samples, we utilize *mixup* [10], which generates new samples by creating a convex combination of two arbitrary samples x_i, x_j with a coefficient $\lambda \sim \text{Beta}(\alpha, \alpha)$:

$$x_{mix} = \operatorname{Mix}_{\lambda}(x_i, x_j) = \lambda x_i + (1 - \lambda) x_j.$$
⁽²⁾

Here, we also use the consistency regularization, but enforce consistency between the predictions on the augmented version of the sample, and the one, which is outside the manifold, but in a close proximity to it. This is achieved by making sure that the original sample's visual appearance is still dominant (i.e., $\lambda > 0.5$). Formally, we target to minimize:

$$\mathbb{E}_{\lambda \sim \operatorname{Beta}(\alpha, \alpha)} \mathbb{E}_{x, x' \sim p(x)} \mathbb{E}_{T \sim p(\tau)} \left\| f_{\theta}(\operatorname{Mix}_{\lambda}(x, x')) - f_{\theta}(Tx) \right\|_{2}^{2}.$$
(3)

Our final regularization term is the interpolation consistency (IC) [11], which also relies on *mixup*, and it encourages a linear behavior of the model's predictions with linear change of the input. We note that from the other regularizers, we obtain almost all the ingredients needed to compute IC term:

$$\mathbb{E}_{\lambda \sim \text{Beta}(\alpha, \alpha)} \mathbb{E}_{x_i, x_j \sim p(x)} \left\| \text{Mix}_{\lambda} (f_{\theta}(x_i), f_{\theta}(x_j)) - f_{\theta}(x_{mix}) \right\|_2^2.$$
(4)

In Semixup, for any pair of samples with or without label x_i and x_j , we apply 2 random augmentations T and T' to x_i , and then compute $x_{mix} = \text{Mix}_{\lambda}(Tx_i, x_j)$ and $p_{mix} = \text{Mix}_{\lambda}(f_{\theta}(Tx_i), f_{\theta}(x_j))$ with $\lambda > 0.5$. To this end, we minimize the unsupervised loss that is a linear combination of the in-manifold term $||f_{\theta}(Tx_i) - f_{\theta}(T'x_i)||_2^2$, the out-of-manifold terms $||f_{\theta}(x_{mix}) - f_{\theta}(Tx_i)||_2^2$, $||f_{\theta}(x_{mix}) - f_{\theta}(T'x_i)||_2^2$. With respect to annotated data, we simply applied *mixup* on them, and used cross-entropy as described in [10].

2.4 Statistical Analyses

To measure the performance of predicting KL grading, we utilized balanced multi-class accuracy (BA), quadratic Cohen kappa score (KC), and mean square error (MSE). Besides, we investigated the ability of early knee OA detection ($KL \ge 2$) by receiver operating characteristic (ROC) curves, area under the ROC curve (AUC), precision-recall (PR) curves, and average precision (AP). For statistical analyses, we used the Wilcoxon signed-rank test [12].

3 Experiments

We compared *Semixup* to interpolation consistency training (ICT) [11], Π model [9], and Mix-Match [13]. All the SL and SSL methods were trained using the same Siamese network presented in 2.2 and augmented by an identical set of transformation settings. The training was done on OAI data, and testing on MOST data.

Results in Figure 1 shows that *Semixup* significantly outperformed the SSL baselines throughout the annotated data settings, expect for the case of 50 annotated samples per KL grade. The fully supervised model achieved a BA of 70.9 ± 0.8 , which is a state-of-the-art (SOTA) performance. However, it required the large data setting with 31,902 annotated samples. Semixup reached BAs of 69.7 ± 0.8 and 71 ± 0.8 with 500 and 1000 annotated images per KL grade, respectively. Statistical analyses showed that the fully supervised model is insignificantly different from the 2 SSL models, having p = 0.054 and p = 0.368, respectively. Finally, Figures 1 and Table 1 consistently show that Semixup performed closely to the SL model in various metrics on the KL grade prediction as well as the early knee OA detection task while requiring over 6 times less annotated samples.



Figure 1: Performance comparisons between *Semixup* and the baseline methods on the MOST dataset. SL (full OAI) indicates the performance of the SL model trained on the full OAI dataset. (a) SL⁺ indicates the SL model, * and ** indicate the statistically significant difference (p < 0.05 and p < 0.001, respectively). (b) + (c) Early knee OA detection (KL ≥ 2).

Method	# annotations	KC	MSE	AUC (KL $\geq 2)$	$AP~(KL \geq 2)$
Semixup	250	0.708	1.080	0.880	0.861
	500	0.789	0.810	0.933	0.916
	2 500	0.877	0.442	0.967	0.956
	5,000	[0.870, 0.884] 0.878	[0.416, 0.466] 0.458	[0.962, 0.972] 0.972	[0.950, 0.962] 0.959
		[0.870, 0.885]	[0.430, 0.487]	[0.968, 0.976]	[0.953, 0.965]
SL (full OAI)	31,922	0.881 [0.873, 0.889]	0.440 [0.414, 0.471]	0.974 [0.969, 0.978]	0.963 [0.958, 0.969]

Table 1: Comparison of our best models trained with *Semixup* against our well-tuned SL model trained on full OAI data.

4 Conclusion

We present a novel SSL method – *Semixup*, which achieves high performance in the task of automatic knee osteoarthritis grading from plain radiographs while being still annotation-efficient. As such, we empirically show that our method requires 6 times less annotations compared to a well-tuned SL model.

5 Broader Impact

DL-based methods are criticized for being data-greedy, which makes small- and medium-scale companies being less competitive compared to the large ones. Our work shows that one can use novel techniques and decrease the requirements for annotated data by a large margin. We hope that the results presented in this paper will be of value to practitioners who aim to develop DL systems for medical imaging applications and beyond.

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