

# Effect of maturation on the bulk optical properties of apple skin and cortex in the 500 to 1850 nm wavelength range

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## Abstract

To facilitate the design of new optical measurement systems for biological systems, the knowledge of light propagation properties is essential. Therefore, the bulk optical properties of skin and cortex of three apple cultivars were studied during maturation, in the 500 nm to 1850 nm range. A clear absorption signature was observed with absorption peaks which can be related to present anthocyanins, chlorophyll, carotenoids and water. During maturation, the skin absorption at 550 nm increased in the bicolored cultivars 'Braeburn' and 'Kanzi', while the absorption at 680 nm decreased in the cortex. Both the bulk scattering coefficient and the anisotropy factor were larger for the skin compared to the cortex tissue. Also during maturation, the skin scattering increased in the two bicolored cultivars, while a general decrease was seen in the apple cortex. Physiological changes during maturation, like cell growth, the formation/degradation of pigments and the formation of a cuticle layer on the skin, may explain the observed evolutions. As a result, using the bulk optical properties, these physiological changes can be monitored and linked to the maturity stage in the orchard, supporting the selective harvest of apples.

31 **Keywords:** Apple, Double Integrating Spheres, Unscattered transmittance, Absorption,  
32 Scattering, Anisotropy factor

33

## 34 **1. Introduction**

35 Optical measurement techniques like visible (vis) and near-infrared (NIR) spectroscopy  
36 (Nicolai et al., 2014), hyperspectral imaging (Boldrini et al., 2012), spatially resolved  
37 spectroscopy (Van Beers et al., 2015) and time resolved spectroscopy (Torricelli et al., 2013)  
38 have shown to be valuable for the nondestructive quality measurement of different types of  
39 intact fruits. Photons entering a material can be absorbed by the molecular bonds, or  
40 scattered at mismatches in the refractive index within the turbid product. The absorption,  
41 therefore, refers to the chemical properties of the material, while the scattering of photons is  
42 related to the (micro)structure (Renfu Lu, 2004). Firmness, crispiness and mealiness are  
43 important fruit quality properties which are associated with the microstructure of the apple  
44 cortex. As the latter influences the light propagation through the tissue, these properties  
45 might be extracted from the signals measured by optical sensors. Yet, in non-destructive  
46 measurements, the photons will first have travelled through the pigmented skin layer before  
47 reaching the apple cortex (Saeys et al., 2008), therefore influencing the obtained signal.  
48 Consequently, the signals measured by optical systems contain information on absorption  
49 and scattering of both the apple skin and cortex. Thus, the correlation between quality  
50 parameters and the optical output is generally based on chemical and physical attributes of  
51 both layers, which complicates the construction and interpretation of calibration models.  
52 Therefore, the optical properties of both apple skin and cortex should be better understood,  
53 to allow light propagation models to be used as a tool for the development of new optical  
54 measurement techniques.

55

56 The propagation of light in turbid media, like biological materials, can be described using the  
57 bulk optical properties (BOP): the bulk absorption coefficient  $\mu_a$ , the bulk scattering coefficient  
58  $\mu_s$  and the angular scattering pattern, represented by the normalized scattering phase  
59 function  $p(\theta)$  (Aernouts et al., 2014). The phase function describes the normalized scattering  
60 probability as a function of the scattering angle  $\theta$ . However, this function is often too complex  
61 to interpret and is, therefore, represented by the anisotropy factor  $g$ , which equals the mean  
62 cosine of the scattering angle (Aernouts et al., 2013). The wavelength dependent scattering  
63 direction of vis/NIR light in biological tissues can often be described with an anisotropy factor  
64 in-between isotropic Rayleigh scattering ( $g = 0$ ) and complete forward scattering ( $g = 1$ )  
65 (Aernouts et al., 2015). The reduced scattering coefficient  $\mu_s'$  combines the bulk scattering  
66 coefficient and the anisotropy factor into a single parameter, which is sufficient to describe  
67 light scattering in the diffusion regime (Tuchin, 2007).

68 Several researchers have tried to estimate the bulk optical properties of apple tissues with  
69 non-destructive optical measurement techniques such as spatially resolved spectroscopy  
70 (Cen et al., 2013; Nguyen Do Trong et al., 2014; Qin et al., 2009; Qin & Lu, 2008) or time  
71 resolved spectroscopy (Cubeddu et al., 2001; Seifert et al., 2014), in combination with  
72 inverse light propagation models (Torricelli et al., 2013). However, it is difficult to estimate the  
73 properties of both skin and flesh simultaneously from such measurements. Moreover, most  
74 studies on apples focused on the estimation of  $\mu_a$  and  $\mu_s'$  (Cen et al., 2013; Lu et al., 2010;  
75 Rowe et al., 2014), while less attention has been given to the actual bulk scattering  
76 coefficient  $\mu_s$  and the scattering anisotropy  $g$ . If *in vitro* characterization of a thin (mm-range)  
77 homogeneous sample slab is feasible, the total reflectance and transmittance can be  
78 measured with integrating spheres, generally accepted as the 'golden standard' method to  
79 estimate BOP for biological tissues (Aernouts et al., 2013; Bashkatov et al., 2005; López-  
80 Maestresalas et al., 2015; Rowe et al., 2014; Saeys et al., 2008; Zamora-Rojas et al., 2013).  
81 Moreover, this technique allows to measure BOP of separate tissue layers. In addition, if the  
82 BOP can be monitored during maturation, changes in the measured BOP could be related to

83 physiological changes during this period. This would enable the design of non-destructive  
84 optical measurement techniques to monitor apple maturity, supporting the selective harvest  
85 and an accurate harvest time prediction.

86

87 Therefore, in this research, the evolution of the bulk optical properties (BOP) of apple skin  
88 and cortex were studied during maturation, as well as their relation with relevant apple quality  
89 and ripeness indicators. Three different apple cultivars, two bicolored (*'Braeburn'* and *'Kanzi'*)  
90 and one green cultivar (*'Greenstar'*), were tested. Reliable double integrating sphere (DIS)  
91 and unscattered transmittance (UT) measurements were used to obtain accurate estimates  
92 for the bulk absorption coefficient  $\mu_a$ , the bulk scattering coefficient  $\mu_s$  and the scattering  
93 anisotropy factor  $g$ .

94

## 95 **2. Materials and methods**

### 96 **2.1 Apple samples**

97 Apples of the cultivars *'Braeburn'*, *'Kanzi'* and *'Greenstar'* were harvested during the 2014  
98 season in Belgium over a timespan ranging from 45 d before to 17 d after the start of the  
99 optimal harvest window. All apples were freshly picked at the 'Centre Fruitier Wallon' in  
100 Merdorp, Belgium (50°38'32.7"N 5°00'13.6"E) on the day of the optical measurements. Due  
101 to the experimental nature of this orchard, not all apples were removed from the tree in the  
102 determined harvest window, and apples were still available for picking until 17 d after the  
103 harvest window started. The Belgian harvest windows for the different cultivars were  
104 determined by the Flanders Centre for Postharvest Technology (VCBT) based on the  
105 evolution of firmness, starch index, soluble solids content (SSC), acidity, size, background  
106 color and Streif index after comparing them to historical records (Peirs et al., 2005). Due to  
107 differences in the harvest window between cultivars, not all apples were measured over the

108 exact same time span. Weekly, 5 apples per cultivar were harvested in the mid-section of the  
109 tree. Accordingly, a total of 50 'Braeburn' apples, 35 'Kanzi' apples and 40 'Greenstar' apples  
110 were picked and the BOP of the skin and fruit cortex were measured.

111 Parallel to the optical characterization of apple skin and cortex, additional apples of the same  
112 cultivars and location were harvested for destructive analysis on the same days. The SSC  
113 (°Brix) of the apple juice was measured using a digital refractometer (PR-101α, Atago,  
114 Tokyo, Japan). As a measure of apple firmness, the maximum force to puncture the apple for  
115 8 mm using an 11 mm diameter plunger at 8 mm/s was determined using a universal testing  
116 machine (LRX, LLOYD Instruments Ltd., Hampshire, UK) (Van Beers et al., 2015). The SSC  
117 and firmness were determined on a set of 20 apples per picking date, while for the starch  
118 conversion value a different set of 10 apples was used, to ensure this measurement was  
119 performed as close as possible to the moment of harvest (Peirs et al., 2005). The starch  
120 conversion value was determined using a starch conversion chart (scale from 1 to 10, Ctifl,  
121 Paris, France). After performing a Lugol's test, which stains the present starch particles using  
122 a  $KI/I_2$  solution on equatorially cut apples, the resulting staining pattern was visually  
123 compared to the chart. Based on the discoloration over the entire surface, a score between  
124 1, a high discoloration, and 10, a low discoloration, was defined (Peirs et al. 2002). All these  
125 parameters were measured by the Flanders Centre for Postharvest Technology (VCBT)  
126 according to the ISO/IEC 17025 standard.

## 127 **2.2 Sample preparation**

128 Both apple skin and cortex samples were optically characterized on the sun exposed side  
129 (blush side), resulting in two measurements per apple. As this side is exposed, it is most  
130 interesting for future field measurements. To only obtain the apple skin, first a slice of 6 mm  
131 in thickness was cut from the apple using a meat slicer (Junior sup 19 mod 30-595A, CAD,  
132 Italy). After this, the excess fruit cortex was scraped off using a scalpel. This remaining skin  
133 layer essentially consisted of the cutin layer plus the epicuticular wax, the epidermis and  
134 probably also some layers of hypodermis cells. Next, these skin samples were cut into disks

135 of 30 mm in diameter and placed in a glass cuvette. The custom-made glass cuvette  
136 consisted of two parallel 1.1 mm thick glass plates (Borofloat33, Schott, Germany) separated  
137 by a spacer of 0.55 mm in thickness. This spacer had a round hole with a diameter of 30  
138 mm. By putting the sample in the provided space, the sample was positioned between the  
139 two 1.1 mm glass plates. As the apple skin samples were typically thinner than 0.55 mm,  
140 demineralized water was added to remove any unwanted air bubbles and to reduce the  
141 refractive index mismatches at the boundaries between the glass plates and the sample. The  
142 apple cortex samples were obtained by slicing the apple at the same place where the skin  
143 sample was removed. The same meat slicer was used to slice the apple cortex to a  
144 thickness of about 0.50 mm. These slices were again loaded in a similar custom made glass  
145 cuvette after which demineralized water was added. For both the apple skin and cortex  
146 samples, the thickness was measured in triplicate using a digital caliper before loading the  
147 samples into the glass cuvette. Also, if obvious defects in one of the samples (e.g. cracks, air  
148 bubbles,...) occurred, this sample was not measured and a new sample was prepared.

149 Once the samples were prepared, the glass cuvette was placed into the sample holder  
150 between the double integrating spheres to measure the total reflectance and transmittance.  
151 All samples were measured directly after preparation, by which drying and browning effects  
152 due to enzymatic reactions were minimized. Repositioning of the sample in a different  
153 measurement path allowed to measure the unscattered transmittance (Aernouts et al., 2013).

### 154 **2.3 Double integrating spheres and unscattered transmittance measurement**

155 The measurement setup used in this research has been described in detail by Aernouts et al.  
156 (2013). In brief, a supercontinuum laser (SC450-4, Fianium Ltd., Southampton, UK) with a  
157 total output power of 4 W and a spectral broadening over the range 450-2400 nm was used  
158 as a light source. By combining this laser light source with a monochromator (Oriel  
159 Cornerstone 260 ¼ m, Newport, Irvine, USA), a monochrome tunable light beam was  
160 obtained. In this research, the wavelength of the illuminating beam was scanned from 500  
161 nm to 1850 nm, with an interval step of 5 nm. During the optical measurements, 10% of the

162 light beam leaving the monochromator was collected by reference detectors to monitor the  
163 stability of the system. For this, a Si detector (PDA100A, Thorlabs Inc., New Jersey, USA)  
164 and a one-stage Peltier-cooled extended-InGaAS detector (PDA10DT-EC, Thorlabs Inc.,  
165 New Jersey, USA) were used for wavelengths below and above 1050 nm, respectively.  
166 Using a flip mirror, the remaining 90% of the monochrome light beam was guided to either  
167 the DIS or the unscattered transmittance measurement path.

168 The DIS measurement path was used to determine the total reflectance ( $M_R$ ) and the total  
169 transmittance ( $M_T$ ) of the sample. For this, the sample was placed in a sample holder  
170 positioned between two *Infragold*<sup>®</sup> coated integrating spheres (RT-060-IG, Labsphere Inc.,  
171 North Sutton, USA): one sphere to measure the total reflectance and one sphere to measure  
172 the total transmittance. Both a Si and extended-InGaAS detector were mounted on each  
173 sphere to measure the obtained diffuse signal over the entire wavelength range from 500 nm  
174 to 1850 nm. The unscattered transmittance ( $M_U$ ) was measured in a separate measurement  
175 path where the sample was placed in an identical sample holder located perpendicular to the  
176 incident collimated light beam (Aernouts et al., 2013). Two detectors, Si and extended-  
177 InGaAs, were placed at a distance of 1.5 m behind the sample to minimize the number of  
178 measured scattered photons.

179 All the detectors in the setup were read by a data acquisition card (NI PCI-6251, National  
180 Instruments Corporation, Texas, USA), while the measurement procedure was programmed  
181 in LabView 8.5 (National Instruments Corporation, Austin, TX, USA) (Aernouts et al., 2013).

## 182 **2.4 Bulk Optical Properties estimation**

183 After measuring  $M_R$ ,  $M_T$  and  $M_U$  using the DIS and unscattered transmittance measurements,  
184 the BOP were estimated using the inverse adding-doubling (IAD) program developed and  
185 optimized by Prahl et al. (1993). To use this inverse estimation code, several setup and  
186 sample related parameters have to be provided to the software. More details on the setup  
187 related parameters, like sphere wall efficiency, diameter of the light spot, refractive index of

188 the cuvette windows, etc. can be found in Aernouts et al. (2013). Another required parameter  
 189 is the sample's refractive index, which is expected to be close to the one of water as it is the  
 190 most important chemical component in apple tissue. Moreover, the wavelength-dependent  
 191 real refractive index of water from Hale & Querry (1973) was used and a wavelength-  
 192 independent constant was added. Saeys et al. (2008) used a refractive index of 1.37 at 589.3  
 193 nm, while the refractive index of water at this wavelength is 1.33 (Hale & Querry, 1973).  
 194 Therefore, based on these findings, a constant of 0.04 was added to the wavelength-  
 195 dependent refractive index of water for both apple skin and cortex.

## 196 **2.5 Data Processing**

197 The BOP values were calculated considering the entire sample cuvette thickness of 0.55  
 198 mm. As the samples were not filling the entire cuvette space, a correction had to be made  
 199 according to the thickness of the used sample. The mean sample thicknesses of three  
 200 repetitions are listed per cultivar in Table 1. As can be seen, the thickness of the apple skin is  
 201 not the same for the different cultivars, while the apple cortex samples were sliced to be  
 202 uniform in thickness, independent of the cultivar.

203 **Table 1 Mean thicknesses with standard deviation of the measured apple skin and cortex samples**

	<b>Skin (mm)</b>	<b>Cortex (mm)</b>
<b>Braeburn</b>	0.213 ± 0.022	0.497 ± 0.035
<b>Kanzi</b>	0.291 ± 0.033	0.497 ± 0.039
<b>Greenstar</b>	0.225 ± 0.024	0.516 ± 0.039

204

205 Knowing the sample thickness, the following equations were used to perform a sample  
 206 specific thickness correction for both the bulk absorption coefficient ( $\mu_a$ ) and the reduced  
 207 scattering coefficient ( $\mu_s'$ ) separately:

$$208 \quad \mu_{a,corrected} = \left( \mu_{a,calculated} - \mu_{a,water} \frac{d_{water}}{d_{total}} \right) \frac{d_{total}}{d_{sample}} \quad (1)$$

209

210

$$\mu'_{s,corrected} = \mu'_{s,calculated} \frac{d_{total}}{d_{sample}} \quad (2)$$

211 Equation (1) shows the thickness correction for  $\mu_a$ , while equation (2) shows the correction

212 performed for  $\mu_s'$ . In these equations, the assumption was made that a perfect two-layered

213 system was obtained with one layer being the sample and the other being water. In both

214 equations,  $d$  stands for the thickness of the different layers, where the total thickness ( $d_{total}$ )

215 corresponds to 0.55 mm. For the correction of the absorption coefficient, the absorption

216 coefficient of water ( $\mu_{a,water}$ ) was measured in the unscattered transmittance path using the

217 same cuvette. As water does not scatter light, the (reduced) scattering coefficient only had to

218 be corrected for the thickness of the sample ( $d_{sample}$ ). The anisotropy factor did not require a

219 correction as it is independent of the actual sample thickness. Finally, the bulk scattering

220 coefficient  $\mu_s$  was derived from  $\mu_s'$  and  $g$  through the similarity relation (Tuchin, 2007):

221

$$\mu_s = \frac{\mu_s'}{(1-g)} \quad (3)$$

222

### 223 **3. Results**

#### 224 **3.1 Apple maturation**

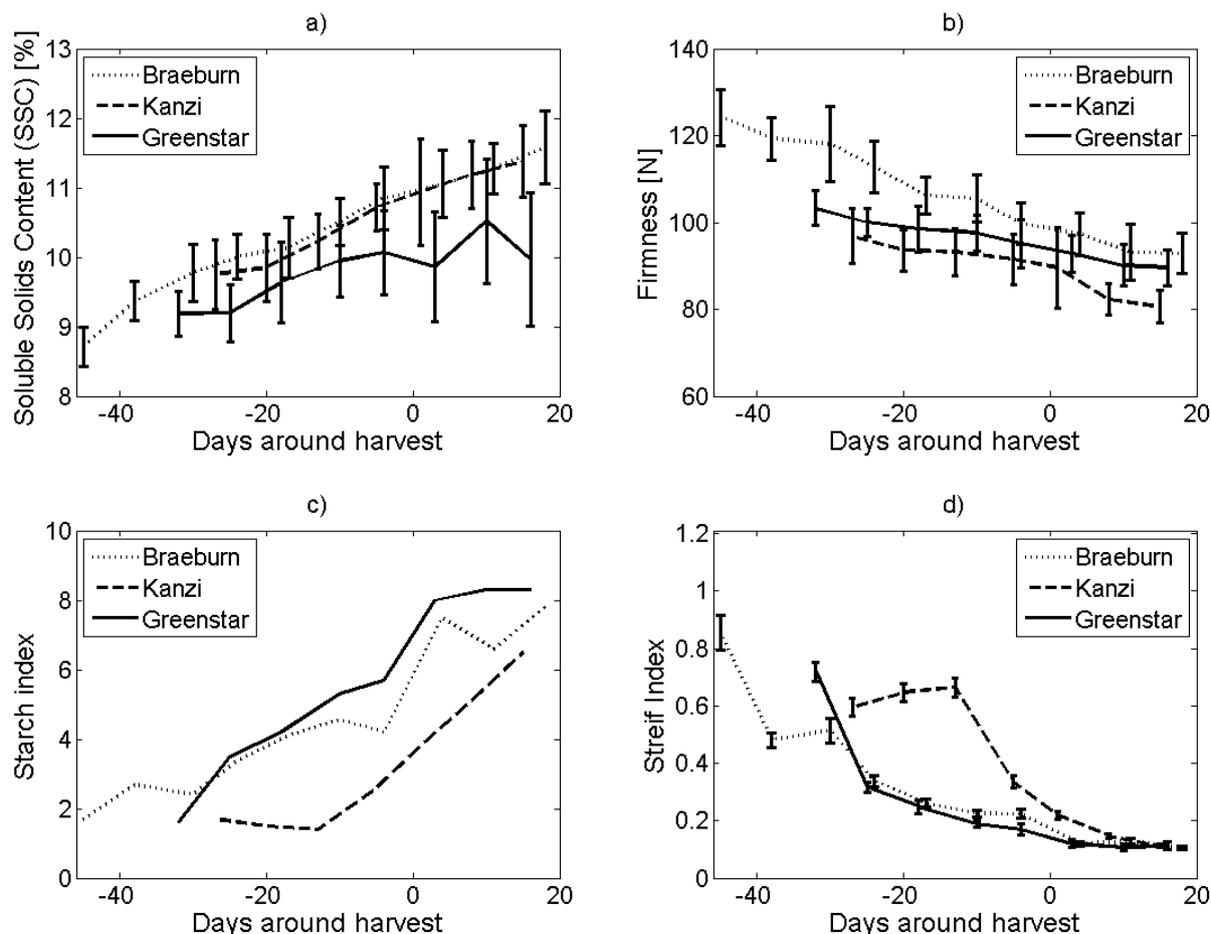
225 In Figure 1a to Figure 1c the evolution of three maturity related parameters (SSC, firmness

226 and starch conversion) is illustrated for the entire measuring period from 45 d before to 17 d

227 after the moment of optimal harvest. The evolution of the Streif index, a maturity index

228 combining these three maturity related parameters, is shown in Figure 1d (Streif, 1996; Van

229 Beers et al., 2015).



230

231 **Fig. 1** The evolution of (a) soluble solids content, (b) firmness, (c) starch conversion values  
 232 and (d) the Streif index, a combination of the parameters in (a)-(b)-(c), during apple fruit  
 233 maturation. The error bars indicate the observed standard deviation.  
 234

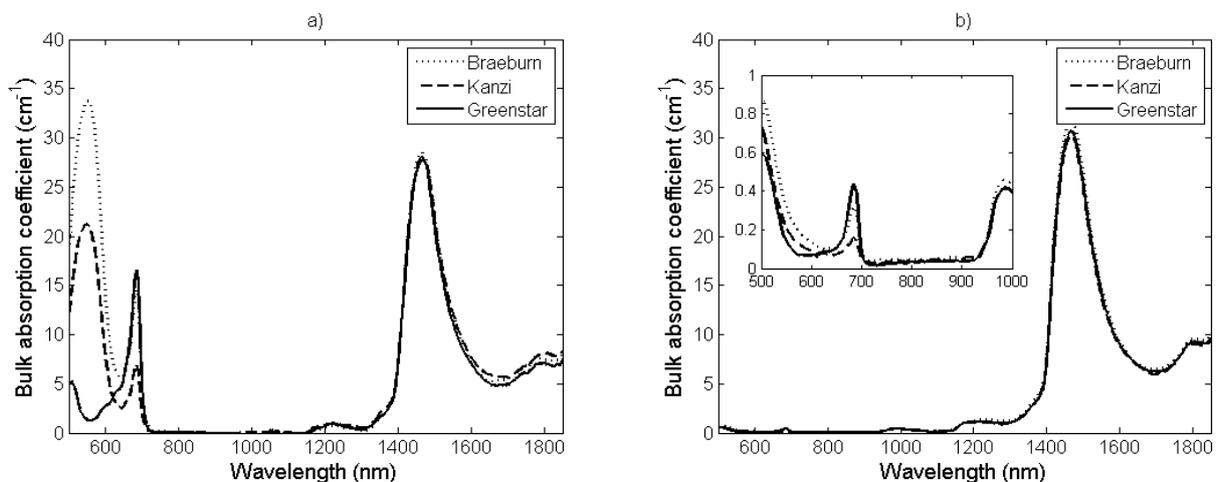
235 Several characteristic trends during maturation can be observed in Figure 1: the SSC values  
 236 (Figure 1a) and starch index (Figure 1c) increase, while the firmness values (Figure 1b) and  
 237 the Streif index (Figure 1d) decrease. However, all measured parameters are location and  
 238 cultivar specific (Peirs et al., 2001). During maturation, the Streif index generally shows a  
 239 sigmoidal trend towards the moment of harvest. This index is often used as a maturity  
 240 parameter which indicates the appropriate time to harvest when it drops below a cultivar  
 241 specific threshold.

242

243

244 **3.2 Bulk optical properties of three apple cultivars**

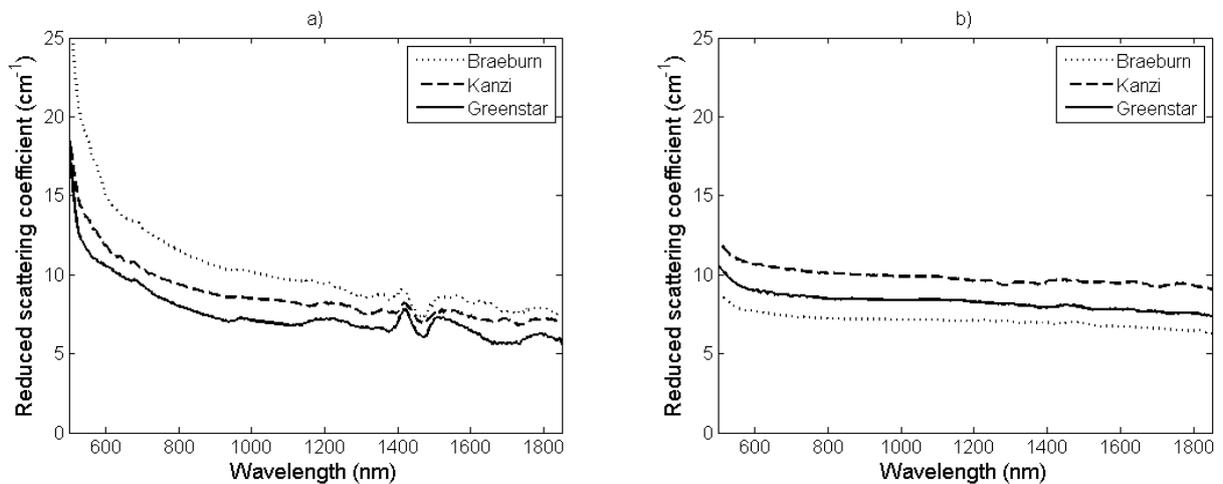
245 In Figure 2 the mean estimated bulk absorption coefficient spectra calculated over four  
246 weeks around harvest (20 apples) are shown for both the apple skin (Figure 2a) and the  
247 apple cortex (Figure 2b) for the three measured apple cultivars. Absorption peaks at 550 nm  
248 and 680 nm occur in the visible part of the spectrum, at which the three cultivars showed  
249 clear differences in absorption. The absorption at 680 nm in the skin tissue (Figure 2a) is  
250 highest in the green cultivar 'Greenstar', with a mean value up to 16.5 cm<sup>-1</sup>. 'Kanzi' has the  
251 lowest absorption at this wavelength with a mean value of 6.9 cm<sup>-1</sup>. Compared to the skin,  
252 the cortex absorption at 680 nm is much lower with mean values up to 0.4 cm<sup>-1</sup> for  
253 'Greenstar' (inset of Figure 2b). At a wavelength of 550 nm, a high absorption was observed  
254 for the bicolored cultivars 'Braeburn' and 'Kanzi'. Other absorption peaks were present in the  
255 NIR part of the spectrum, at 970 nm, 1200 nm and 1450 nm.



256  
257 **Fig. 2** Mean bulk absorption coefficient  $\mu_a$  spectra for (a) the skin and (b) the cortex tissue of  
258 three apple cultivars during four weeks around harvest. The inset figure shows the  
259 absorption coefficient spectra for apple cortex in the 500-1000 nm range.  
260

261 In Figure 3, the mean measured reduced scattering coefficient ( $\mu_s'$ ) spectra during four  
262 weeks around harvest are visualized for both apple skin (Figure 3a) and cortex (Figure 3b). It  
263 is clear from Figure 3 that the reduced scattering coefficient decreases exponentially with  
264 increasing wavelength, which is typical for biological tissues (Bashkatov et al., 2005). This  
265 evolution is more pronounced in the apple skin compared to the apple cortex, especially in

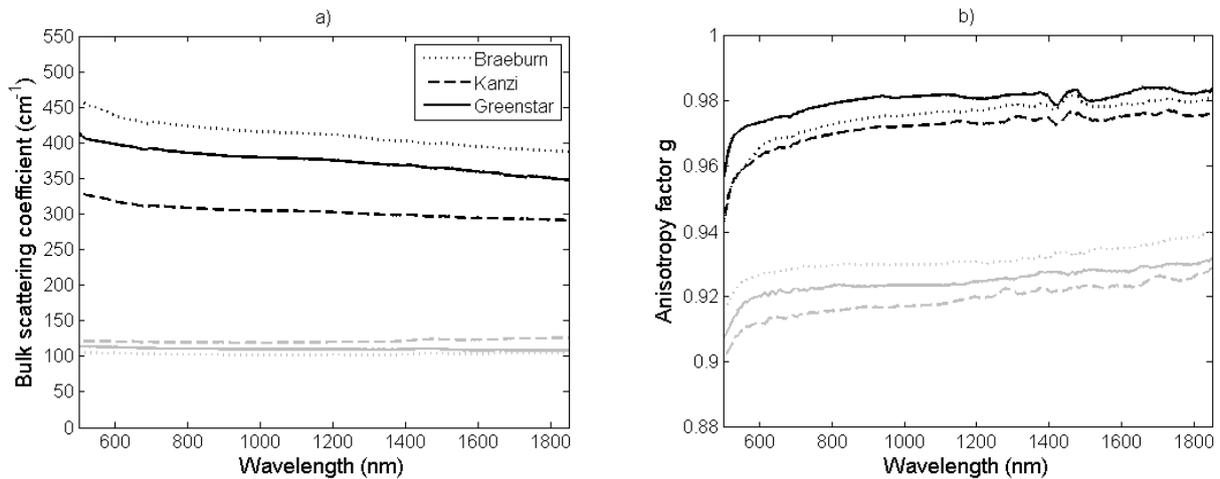
266 the visible region of the spectrum. Moreover, a flatter course is seen for the  $\mu_s'$  spectra of  
 267 apple cortex with values around  $10 \text{ cm}^{-1}$ . Some small cultivar differences are present in both  
 268 the skin and cortex tissue. Especially the 'Braeburn' cultivar shows a difference over the  
 269 entire wavelength range, where the  $\mu_s'$  of the skin is higher compared to the other cultivars,  
 270 while for the apple cortex it is lower. For 'Greenstar', the  $\mu_s'$  values of the skin and cortex  
 271 were similar for wavelengths above 1000 nm. Moreover, in this region, the reduced  
 272 scattering coefficient of 'Kanzi' cortex is even higher than that of the skin.



273 **Fig. 3** Mean reduced scattering coefficient  $\mu_s'$  of (a) apple skin and (b) cortex tissue of three  
 274 apple cultivars during four weeks around harvest.  
 275  
 276

277 The accurate measurement of the unscattered transmittance in this study resulted in a robust  
 278 estimation of both the bulk scattering coefficient  $\mu_s$  (Figure 4a) and the anisotropy factor  $g$   
 279 (Figure 4b).

280



281  
 282 **Fig. 4** (a) Mean bulk scattering coefficient  $\mu_s$  and (b) anisotropy factor  $g$  of both the skin  
 283 (black lines) and cortex tissue (grey lines) of three apple cultivars during four weeks around  
 284 harvest.  
 285

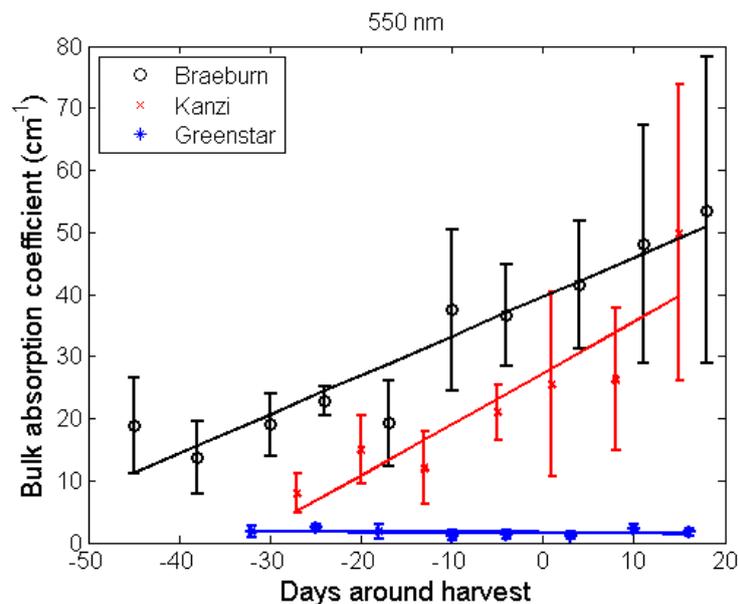
286 In Figure 4, a clear difference can be noticed between the scattering properties of apple skin  
 287 (black lines) and cortex (grey lines). The  $\mu_s$  of the skin decreases with increasing wavelength,  
 288 while the  $\mu_s$  of the cortex is more wavelength independent. The anisotropy factor of both the  
 289 apple skin and cortex shows an increase with increasing wavelength, typical for biological  
 290 tissues (Jacques, 2013). The apple skin samples have a high bulk scattering coefficient, with  
 291 mean values up to  $425 \text{ cm}^{-1}$  at 800 nm. This is significantly higher than for the apple cortex,  
 292 which has mean values up to  $120 \text{ cm}^{-1}$  at the same wavelength. When comparing the three  
 293 different cultivars, ‘*Kanzi*’ differs the most from the other two cultivars. The  $\mu_s$  of the skin is  
 294 significantly lower, with a value of  $308 \text{ cm}^{-1}$  at 800 nm, compared to  $386 \text{ cm}^{-1}$  and  $423 \text{ cm}^{-1}$   
 295 for ‘*Greenstar*’ and ‘*Braeburn*’, respectively. For the cortex samples, an opposite trend can  
 296 be noticed, as ‘*Kanzi*’ shows the highest  $\mu_s$ , going up to  $119 \text{ cm}^{-1}$  at 800 nm.

297 Similar to the bulk scattering coefficient, a significant difference in the anisotropy factor ( $g$ )  
 298 between apple skin and cortex can be observed in Figure 4b. Both apple skin and cortex  
 299 have an anisotropy factor close to one, which indicates a high forward scattering. The results  
 300 indicate that the apple skin is more forward scattering compared to the cortex, with a  $g$ -value  
 301 at 800 nm of 0.97 for the skin compared to 0.93 for the cortex.

### 302 3.3 Evolution of optical properties during maturation

#### 303 3.3.1 Absorption properties

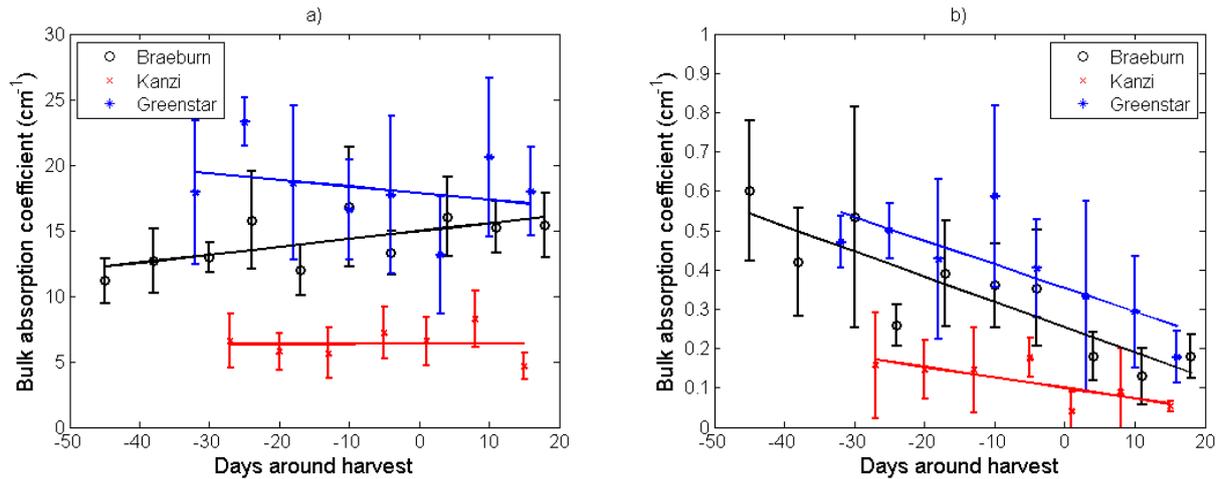
304 In Figure 5, the evolution of the apple skin's bulk absorption coefficient ( $\mu_a$ ) at 550 nm over  
305 the measured maturation period is illustrated. The solid lines indicate the observed trends in  
306 the three different apple cultivars, while the error bars indicate the corresponding standard  
307 deviations.



308 **Fig. 5** Bulk absorption coefficient at 550 nm during maturation for the skin of three apple  
309 cultivars. The error bars indicate the standard deviation.  
310  
311

312 From Figure 5 it can be observed that the absorption coefficient values at 550 nm for the skin  
313 samples increased significantly ( $p < 0.01$ ) towards the moment of harvest (and afterwards) in  
314 'Braeburn' and 'Kanzi' apple cultivars. A large standard deviation can be observed for both  
315 red cultivars, while the 'Greenstar' cultivar shows much lower variations. Moreover, no  
316 significant increase in the absorption at 550 nm was seen in this green cultivar.

317 The evolution of the absorption coefficient at 680 nm is shown in Figure 6 for both the apple  
318 skin (Figure 6a) and cortex (Figure 6b).

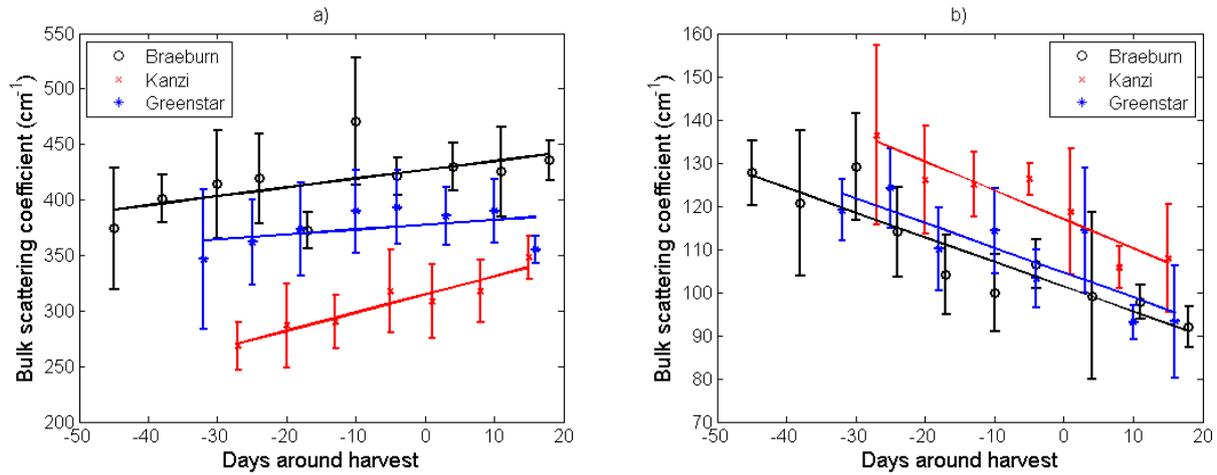


319 **Fig. 6** Bulk absorption coefficient at 680 nm during maturation for both (a) the skin and (b)  
 320 cortex of three apple cultivars. The error bars indicate the standard deviation.  
 321  
 322

323 While a clear upwards evolution in the skin absorption at 550 nm could be observed for  
 324 'Kanzi' and 'Braeburn', the change in absorption by the skin at 680 nm is much less obvious  
 325 (Figure 6a). Only a significant change ( $p < 0.01$ ) was found for 'Braeburn' skin samples.  
 326 Although non-significant ( $p = 0.331$ ), 'Greenstar' showed a slightly decreasing trend (Figure  
 327 6a). In the apple cortex, a significant downward trend in the  $\mu_a$  at 680 nm was observed in  
 328 both 'Kanzi' ( $p < 0.05$ ) and 'Greenstar' ( $p < 0.01$ ). 'Braeburn' also showed this downwards trend  
 329 in Figure 6b, but the observed trend was not statistically significant ( $p = 0.0664$ ).

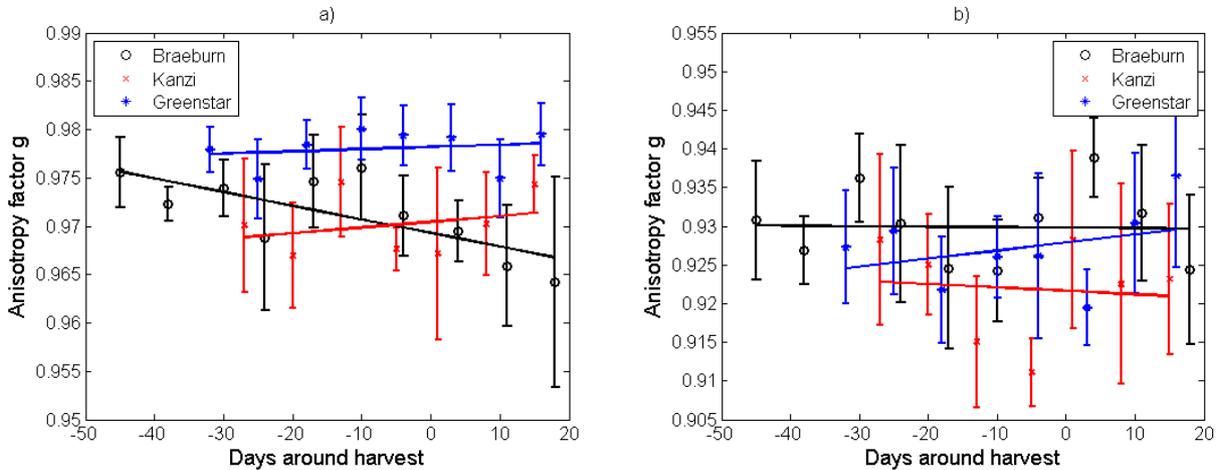
### 330 3.3.2 Scattering properties

331 In Figure 7 and Figure 8 the evolution of the bulk scattering coefficient  $\mu_s$  and the scattering  
 332 anisotropy factor  $g$  during maturation is illustrated. The scattering trends are shown for one  
 333 specific wavelength (850 nm), as both  $\mu_s$  and  $g$  are mostly wavelength-independent for  
 334 wavelengths above 700 nm.



335  
 336 **Fig. 7** Bulk scattering coefficient at 850 nm during maturation for both (a) the skin and (b) the  
 337 cortex of three apple cultivars. The error bars indicate the obtained standard deviation.  
 338

339 In Figure 7a, an upward trend in the skin's bulk scattering coefficient with maturation can be  
 340 observed, while a downward trend is observed for the apple cortex (Figure 7b). All of these  
 341 trends were significant ( $p < 0.05$ ) except for 'Greenstar' skin. In 'Greenstar' skin, first an  
 342 increase is noticed, while around harvest, the values start to decrease.



343  
 344 **Fig. 8** Anisotropy factor  $g$  at 850 nm during maturation for both (a) the skin and (b) the cortex  
 345 of three apple cultivars. The error bars indicate the obtained standard deviation.  
 346

347 Figure 8 indicates that, during maturation, no consistent evolutions in the anisotropy factor  
 348 could be observed for the apple skin and cortex for any of the three cultivars. Only a  
 349 significant change ( $p < 0.01$ ) was noticed in anisotropy factor for the apple skin of 'Braeburn'

350 apples. This decreasing trend is mainly present after the optimal point of harvest, whereas  
351 before this point no large change could be observed.

352 Finally, the trends for the reduced scattering coefficient  $\mu_s'$  during maturation were studied as  
353 well (figure not shown). This coefficient is a combination of  $\mu_s$  and  $g$  (equation (3)) and  
354 therefore shows a combined effect of both parameters. Like  $\mu_s$ , the reduced scattering  
355 coefficients of the fruit cortex showed a significant downwards trend ( $p < 0.05$ ) for all cultivars.  
356 However, in the apple skin, only a significantly increasing trend was observed in 'Braeburn'.

357

## 358 **4. Discussion**

### 359 **4.1 Apple bulk optical properties**

360 Figure 2 illustrated the main absorption peaks for both the apple skin and cortex. Based on  
361 literature, these absorption peaks are most likely related to the presence of carotenoids  
362 (around 500 nm), anthocyanins (550 nm – 600 nm), chlorophyll (mainly *chlorophyll a* at 678  
363 nm) and water (Lancaster et al., 1994; Merzlyak et al., 2003). The most important  
364 anthocyanin responsible for the red apple color is cyanidin 3-O-galactoside (Espley et al.,  
365 2007; Lancaster et al., 1994), while known carotenoids in the apple skin are lutein,  
366 violaxanthin, neoxanthin and  $\beta$ -carotene (Delgado-Pelayo et al., 2014). While carotenoids,  
367 anthocyanins and chlorophyll are the main pigments in the apple skin, also the cortex  $\mu_a$   
368 spectra contained features related to the presence of chlorophyll and carotenoids (inset in  
369 Figure 2b). From literature, water is known to have prominent absorption peaks in the NIR  
370 part of the spectrum, respectively at 970 nm, 1200 nm and 1450 nm (Hale & Querry, 1973).  
371 Lipids in the cuticular wax layer on the apple skin can absorb light in the region around 1200  
372 nm (Veraverbeke et al., 2005).

373 As 'Greenstar' is a green cultivar, very little anthocyanins are formed in the apple skin, which  
374 could explain the low absorption at 550 nm. In contrast, both bicolored cultivars ('Kanzi' and  
375 'Braeburn') showed high absorption at 550 nm with mean values up to  $34 \text{ cm}^{-1}$  for 'Braeburn'.

376 Additionally, in the skin of 'Greenstar' and the cortex of all three cultivars, substantial  
377 absorption can be noticed around 500 nm, which might be attributed to the presence of  
378 carotenoids (Merzlyak et al., 2003).

379 When comparing the obtained bulk absorption coefficients with the values reported in  
380 literature, some differences can be noticed. Cubeddu et al. (2001) found a maximal  
381 absorption coefficient at 680 nm of  $0.25 \text{ cm}^{-1}$  in 'Granny Smith' using time resolved  
382 spectroscopy. With spatially resolved spectroscopy, maximal chlorophyll peaks of  $0.6 \text{ cm}^{-1}$   
383 and  $2.5 \text{ cm}^{-1}$  were obtained in 'Golden Delicious' and 'Braeburn' apples respectively (Nguyen  
384 Do Trong et al., 2014; Qin & Lu, 2008). However, these techniques measured the whole  
385 apple, with the former penetrating deeper than the latter, therefore showing the bulk effect of  
386 both the skin and cortex absorption in a different ratio. Moreover, the estimation of optical  
387 properties involves modeling the light propagation into the tissue using Monte Carlo  
388 simulations (Qin & Lu, 2009), the diffusion approximation of the radiative transfer equation  
389 (Cubeddu et al., 2001) or a metamodeling approach (Aernouts et al., 2015; Nguyen Do  
390 Trong et al., 2014). Therefore, the obtained BOP also depend on the viability and robustness  
391 of the used modeling approaches, as well as on the assumptions made by these techniques.  
392 For the estimation of the BOP of apple, both Saeys et al. (2008) and Rowe et al. (2014) used  
393 a single integrating sphere measurement. Like the results obtained in this research, Saeys et  
394 al. (2008) found a  $\mu_a$  around 680 nm between  $5$  and  $10 \text{ cm}^{-1}$  for 'Braeburn' apple skin, while  
395 higher absorption values up to  $30 \text{ cm}^{-1}$  were observed at a wavelength of 500 nm. For the  
396 apple cortex, mainly water peaks were noticed, while no clear absorption peaks were present  
397 in the visible region of the spectrum (Saeys et al., 2008). However, similar to what was seen  
398 in Figure 2, Rowe et al. (2014) found an absorption peak at 680 nm of about  $0.1 \text{ cm}^{-1}$  in the  
399 cortex of *Royal Gala* apples at commercial maturity.

400 The obtained reduced scattering coefficients in Figure 3 were consistent with the values  
401 reported in literature. Other researchers found  $\mu_s'$  values for different cultivars ranging  
402 between  $10 \text{ cm}^{-1}$  and  $20 \text{ cm}^{-1}$  (Cen et al., 2013; Cubeddu et al., 2001; Nguyen Do Trong et

403 al., 2014; Qin & Lu, 2008; Rowe et al., 2014; Saeys et al., 2008; Seifert et al., 2014). When  
404 looking at the skin and cortex tissue separately, Saeys et al. (2008) found a larger  $\mu_s'$  for skin  
405 tissue with values up to  $40 \text{ cm}^{-1}$  at 600 nm, calculated with a fixed anisotropy factor.

406 The bulk scattering coefficient  $\mu_s$  showed clear differences between the apple skin and cortex  
407 tissue (Figure 4a), which might be attributed to the cell structure in both tissue types. It was  
408 found by other researchers that the apple cortex cells are much larger than the compact  
409 epidermis cells (Herremans et al., 2013; Schotsmans et al., 2004; Bain & Robertson, 1951).  
410 Moreover, the large cortex cells are separated by big air pores, causing a more spacious  
411 structure (Herremans et al., 2013). Consequently, the smaller epidermis and hypodermis  
412 cells (Verboven et al., 2008, 2013) have a denser concentration of scattering particles. This  
413 cell size difference between the cortex and skin tissue could also explain the steeper  
414 decreasing trend in the skin samples, as according to Mie scattering theory this is typically  
415 related to smaller scatterers (Aernouts et al., 2015). Saeys et al. (2008) also reported  
416 differences between the scattering coefficient of apple skin and cortex, but the actual values  
417 were considerably smaller, with a  $\mu_s$  for skin ranging between  $100 \text{ cm}^{-1}$  and  $150 \text{ cm}^{-1}$ , while  
418 the  $\mu_s$  for apple cortex ranged from  $30 \text{ cm}^{-1}$  to  $50 \text{ cm}^{-1}$ . The suboptimal configuration for  
419 unscattered transmittance measurements used in that study, most likely resulted in the  
420 detection of scattered photons and consequently an underestimation of the extinction by the  
421 sample (Aernouts et al., 2013). This is most likely the reason why  $\mu_s$  and  $g$  were  
422 underestimated in the study of Saeys et al. (2008).

423 The observed differences in the anisotropy factor  $g$  of skin and cortex (Figure 4b) may be  
424 attributed to differences in the main scattering particles. The higher  $g$  values for the skin  
425 samples suggest larger scattering particle sizes. Contradictory, the steeper descend of the  
426 skin's bulk scattering coefficient observed earlier would indicate the presence of mainly small  
427 scattering particles. However, the Mie scattering theory assumes spherical scattering  
428 particles (Aernouts et al., 2015), while many of the scattering particles in plant cells are far  
429 from spherical (Konarska, 2014; Stevenson et al., 2006; Verboven et al., 2013). This could

430 possibly be the reason why the observed relation between the bulk scattering coefficient and  
431 anisotropy factor spectra was not consistent with the Mie theory. Saeys et al. (2008) also  
432 found that the anisotropy factor of the apple skin was higher compared to the apple cortex.  
433 Moreover, Baranyai et al. (2009) found anisotropy factor values around 0.95 at 785 nm  
434 during cool storage of 'Pinova' and 'Elstar' apples.

#### 435 **4.2 Evolution of optical properties during maturation**

436 To monitor  $\mu_a$  during maturation, two wavelengths, 550 nm and 680 nm, were followed,  
437 because these have been reported to correspond to the absorption peaks of anthocyanins  
438 and chlorophyll, respectively (Lancaster et al., 1994; Merzlyak et al., 2003). In Figure 5,  
439 showing the evolution of the absorption at 550 nm, a large standard deviation can be  
440 observed. This is probably a result of the high variation in anthocyanin concentrations in  
441 apple skin (Singha et al., 1991). However, the observations made are in line with other  
442 publications on the increase of the anthocyanin concentration during maturation (Awad et al.,  
443 2001; Lister et al., 1996; Reay et al., 1998). Furthermore, several researchers have  
444 suggested a decrease in the chlorophyll concentration during maturation (McGlone et al.,  
445 2002; Mir et al., 2001; Reay et al., 1998; Rutkowski et al., 2008; Song et al., 1997). In Figure  
446 6, showing the absorption at 680 nm during maturation, no significant trends can be  
447 observed for the skin samples, except for a significant upward trend in the skin samples of  
448 the 'Braeburn' cultivar. However, for the cortex samples of all three cultivars a significant  
449 decreasing trend can be observed.

450 The scattering of light passing through apple tissue is caused by the scattering particles  
451 present, such as cell walls, air pores and cellular content (e.g. vacuoles, starch granules,  
452 chloroplasts) (Lu, 2004; Nicolai et al., 2014; Rowe et al., 2014). For the apple cortex samples  
453 of all three cultivars the bulk scattering coefficient values at 850 nm, shown in Figure 7b,  
454 decreased significantly during maturation. A possible explanation for this decrease can be  
455 found in the apple development. In a first stage of fruit development, cells are rapidly

456 dividing, while the actual size of the apple does not change much. However, during the  
457 maturation period considered in this research, the cell division stops after which the newly  
458 differentiated cells start to elongate (Bain & Robertson, 1951; Grierson, 2001; Seifert et al.,  
459 2014). During this cell elongation, cells and pores both become larger, but their total number  
460 does not change. As an effect, the overall apple diameter increases without the formation of  
461 new cells. Therefore, less cell walls and air pores will be encountered by the light on a  
462 volume basis. This could explain the decreasing scattering coefficient observed. Moreover,  
463 during maturation starch is converted into sugars (Smith et al., 2005) resulting in less starch  
464 granules and thus scattering particles in the cortex over time. In the skin, an opposite  
465 evolution of the scattering properties was observed over time than the one observed for the  
466 cortex (Figure 7a). However, a similar evolution during apple development is observed  
467 compared to the fruit flesh, where during this period the cell division ceases, followed by a  
468 stage of elongation and flattening of the cells during maturation. However, in contrast to the  
469 cortex cells, the epidermal cells excrete a waxy, cutinous material during this elongation  
470 stage (Grierson, 2001). This cuticle is a heterogeneous polymer of fatty acids overlaid with a  
471 layer of wax in which the epidermal cells are embedded and which can even further develop  
472 after harvest (Dominguez et al., 2011; Grierson, 2001). In a study performed by Solovchenko  
473 & Merzlyak (2003), the cuticle layer of apples was found to have a significant scattering  
474 effect, which was observed as a wavelength dependent increase of the cuticular optical  
475 depth. This could be the reason for the increase in the apple skin  $\mu_s$  during maturation.

476 Finally, the absence of changes in the anisotropy factor  $g$  observed in Figure 8, could confirm  
477 the previous observations made for  $\mu_s$ . Moreover, it was suggested that cell growth could be  
478 responsible for the changes in scattering, as less scatterers will be encountered for a similar  
479 volume of fruit, while geometry and size of the scattering particles will most likely be  
480 constant. For example, chloroplasts stay present in the epidermal cells during maturation,  
481 though changes occur in the concentration of chlorophyll. More in detail, the chloroplasts  
482 convert into gerontoplasts, by which also structural modifications of the thylakoid membranes

483 occur inside the organelle. The envelope of the chloroplast, however, remains intact (Biswal  
484 et al., 2011). As a result, the main scattering particles likely remain present and the  
485 anisotropy factor remains constant.

### 486 **4.3 General remarks**

487 One of the requirements for the IAD calculations is that the measured samples are  
488 homogeneous (Prahl et al., 1993). However, the measured apple samples can have small  
489 irregularities, like air pores, color changes, lenticels, etc. Although this effect on the eventual  
490 estimation of BOP is believed to be limited, more complex modelling strategies like the  
491 meshed Monte Carlo method (Watté et al., 2015a), could provide an added value here.

492 Herremans et al. (2013) showed that the cortex cells of 'Braeburn' apples have an average  
493 length of 0.299 mm and a width of 0.2175 mm. As the cortex sample thicknesses were only  
494 about 0.5 mm (Table 1), only two to four cell layers were sampled, of which two were  
495 probably damaged by the cutting procedure. Therefore, it can be expected that the cutting  
496 process might have influenced the obtained results. Nevertheless, according to Mie theory  
497 the main scattering particles in the vis/NIR region of the spectrum are the cell organelles  
498 (Aernouts et al., 2014). Thus, the measured BOP of the apple cortex samples are expected  
499 to be valid. Moreover, as variation was also present in the results of the measured skin  
500 samples, which were not cut, the effects of biological variability might have been higher in  
501 comparison to the introduced effects of cutting.

502 The obtained results give valuable information to go towards future applications for fruit  
503 quality monitoring. The observed trends in BOP might be related to the observed quality  
504 changes in Figure 1. However, more measurements on a large set of samples are essential  
505 for building robust calibration models. To achieve this, novel optical measurement techniques  
506 should be designed which can measure the BOP in a fast and non-destructive way. Light  
507 propagation models can be used for *in silico* design of these techniques and the BOP of  
508 apple skin and cortex are essential inputs for this. Simulations based on these models will

509 enable the development and optimization of both sensors and data processing techniques  
510 (Watté et al., 2015a; Watté et al., 2015b). These novel sensors could then be used for the  
511 monitoring of fruit quality parameters and would promote the evaluation of fruit maturity for  
512 picking decisions in mechanical harvesting applications.

513

## 514 **5. Conclusions**

515 The absorption coefficient ( $\mu_a$ ) showed absorption features of carotenoids (500 nm),  
516 anthocyanins (550 nm), chlorophyll (678 nm), wax lipids (1200 nm) and water (970 nm, 1200  
517 nm and 1450 nm). Most pigments were present in the apple skin, with a maximal absorption  
518 by anthocyanins going up to  $50 \text{ cm}^{-1}$ . In comparison to the bicolored cultivars '*Braeburn*' and  
519 '*Kanzi*', a larger absorption by chlorophyll was observed in the green cultivar '*Greenstar*',  
520 while nearly no anthocyanin absorption could be observed. During maturation, a significant  
521 increase in the absorption by anthocyanins was seen in the skin of bicolored cultivars. In  
522 contrast, the absorption by chlorophyll showed no clear changes in the apple skin, while in  
523 the apple cortex of '*Kanzi*' and '*Greenstar*' a significant decrease was noticed. A clear  
524 difference between the scattering properties of apple skin and cortex was observed. The  
525 apple skin was more highly scattering compared to the apple cortex. Both the skin and cortex  
526 were found to be highly forward scattering, with respective anisotropy factors of 0.97 and  
527 0.93 at 800 nm. All cultivars showed a decrease in the bulk scattering coefficient of the apple  
528 cortex during maturation, while it increased in the apple skin of the '*Kanzi*' and '*Greenstar*'  
529 cultivars. While clear changes were seen in the scattering, the anisotropy factor only  
530 changed in the skin of '*Braeburn*' apples. Therefore, it was hypothesized that the shape and  
531 size of the scattering particles are hardly changing during maturation.

532

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