PhAc-ALGP-Dox, a novel anti-cancer prodrug with targeted activation and improved therapeutic index

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Running Title

Unique MoA of PhAc-ALGP-Dox enhances efficacy and safety

Disclosure of Potential Conflicts of Interest

AC, LVH, PP, NDG, MDP, TJ, MP, MD, OD, GR and NK are employees of CoBioRes NV. PS and MM have an institutional grant from CoBioRes NV. No potential conflicts of interest were disclosed by the other authors.

This work was supported by grants from the Fund for Scientific Research Flanders (HBC-2016-0887 and HBC-2017-1005).

ABSTRACT

Clinical use of doxorubicin (Dox) is limited by cumulative myelo- and cardiotoxicity. This research focuses on the detailed characterization of PhAc-ALGP-Dox, a targeted tetrapeptide prodrug with unique dual-step activation mechanism, designed to circumvent Dox-related toxicities and ready for upcoming clinical investigation. Coupling Dox to a phosphonoacetyl (PhAc)-capped tetrapeptide forms the cell-impermeable, inactive compound, PhAc-ALGP-Dox. After extracellular cleavage by tumor-enriched thimet oligopeptidase-1 (THOP1), a cell-permeable but still biologically inactive dipeptide-conjugate is formed (GP-Dox), which is further processed intracellularly to Dox by fibroblast activation protein-alpha (FAP α) and/or dipeptidyl peptidase-4 (DPP4). *In vitro*, PhAc-ALGP-Dox is effective in various 2D and 3D-cancer models, while showing improved safety towards normal epithelium, hematopoietic progenitors and cardiomyocytes. *In vivo*, these results translate into a 10-fold higher tolerability and 5-fold greater retention of Dox in the tumor microenvironment compared to the parental drug. PhAc-ALGP-Dox demonstrates 63 to 96% tumor growth inhibition in preclinical models, an 8-fold improvement in efficacy in patient-derived xenograft (PDX) models, and reduced metastatic burden in a murine model of experimental lung metastasis, improving survival by 30%. The current findings highlight the potential clinical benefit of PhAc-ALGP-Dox, a targeted drug-conjugate with broad applicability, favourable tissue biodistribution, significantly improved tolerability and tumor growth inhibition at primary and metastatic sites in numerous solid tumor models.

INTRODUCTION

Conventional chemotherapy is currently indispensable in most oncological treatments. However, clinical application is often limited by dose-related side effects and therefore, reducing systemic toxicity and improving therapeutic index remains an important challenge. With that purpose, different formulations have been optimized to decrease drug clearance, increase therapeutic efficacy and/or modulate systemic toxicity. Alternatively, strategies masking cytotoxicity and selectively delivering payloads into cancer cells, such as antibody-drug conjugates (ADC), have been applied. However, ADCs remain hampered by uncontrolled payload release, immunogenicity, poor tumor penetration and resistance (1).

Another elegant therapeutic approach are protease-activated conjugates (PAC). Here, the payload is attached to a protease-cleavable linker, making the molecule inactive prior to cleavage by the target protease. This reduces the size of the molecule compared to ADCs, potentially improving tumor penetration and reducing immunogenicity. Moreover, efficient hydrolysis and selective payload activation is guaranteed by swift recognition of the peptidic moiety by tumor specific proteases.

Dox is one of the most effective anticancer drugs used for treatment of a broad range of solid tumors. However, clinical applicability has long been limited due to severe dose-dependent cardio- and myelotoxicity. DTS-201 (CPI0004Na) consists of the tetrapeptide N-succinyl- β -alanyl-L-leucyl-L-alanyl-L-leucine covalently linked to Dox. DTS-201 is stable in blood but cleavable by specific peptidases present in the tumor environment (2,3). DTS-201 demonstrated good efficacy and lower toxicity compared to Dox in preclinical models (4,5). In patients, DTS-201 was well tolerated up to 400 mg/m², corresponding to 3.75-fold the standard dose of Dox and showed encouraging results in clinical trials (6).

Following the same rationale, PhAc-ALGP-Dox was developed as an advanced tetrapeptidic conjugate of Dox. The payload is coupled to a phosphonoacetyl-capped L-Alanyl-L-Leucyl-L-glycyl-L-prolyl peptide, rendering it inactive and preventing cellular uptake. Once in the tumor vicinity, PhAc-ALGP-Dox is metabolized to a cell-permeable but biologically inactive intermediate, GP-Dox, which is further cleaved intracellularly by FAP α and/or DPP4 exopeptidases, liberating Dox exclusively at the tumor (7).

In this study, the unique mode of activation, preclinical evidences of the *in vitro* potency and selectivity of PhAc-ALGP-Dox are unraveled, together with the antitumor efficacy in clinically relevant xenograft and PDX models spanning a variety of indications.

METHODS

Drugs, recombinant enzymes and inhibitors

Doxorubicin-HCl was acquired from LC-Labs (D-4000-500mg). PhAc-ALGP-Dox was synthesized by WuXi AppTec (China). Following recombinant human enzymes were purchased from R&D Systems (Bio-technique, UK): THOP1 (3439-ZNC, 0.1 µg/ml), CD10 (1182-ZNC, 0.08 µg/ml), NLN (4308-SE, 0.8 µg/ml), FAPα (3715-SE, 0.04 µg/ml) and DPP4 (9168-SE, 0.04 µg/ml). Following inhibitors were used to block activity of endogenous peptidases: THOP1 was specifically inhibited with Cpp-AAF-pAB (100 µM Bachem), THOP1 and CD10 were blocked with JMV-390 (10 µM, Tocris #2575, UK), DPP4 and FAPα was constrained using talabostat (=PT-100, 10 µM, Tocris #3719), while FAPi (MedChemExpress, HY100684, US) was used to specifically inhibit FAPα.

Peptidase cleavage assay (PCA) and LC-MS/MS

Two µM PhAc-ALGP-Dox or DTS-201 were dissolved in PCA buffer (150 mM NaCl, 50 mM Tris, 1% BSA, pH 7.5, 37°C). The reaction was initiated through addition of recombinant enzymes at equi-active concentrations ($t=0$). Samples were snap frozen in liquid nitrogen at $t = 1, 5, 15, 30, 60, 240$ and 960 min and stored at -80°C . Prior to analysis, samples were defrosted and mixed with ice cold MeOH/ CH_3CN containing ^{13}C -Dox (1:5) to remove salts, proteins and stop enzymatic reactions. Samples were vortexed and centrifuged (12,000 rpm, 10 min at 4°C). Supernatants were transferred to a matrix tube for LC-MS/MS using an Acquity Class I Xevo TQS micro (Waters Corporation, Manchester, UK). Five mM ammonium formate (pH 3.75) and 5% aqueous CH_3CN 5 mM ammonium formate (pH 3.75) were used as mobility phase. Electron-spray-ionization and subsequent MS/MS analysis was performed using the Xevo TQ-S at a source temperature of 150°C and cone gas flow of 50 l/hr. Desolvation gas flow was 1200 l/hr. Half-life ($t_{1/2}$) was calculated using the Xlfit™ software (IBDS Ltd). Hundred percent of parent compound was extrapolated from the curve-fit to determine time zero concentrations.

Cell lines

Human cell lines and rat cardiomyoblasts (H9C2) were acquired from American Type Culture Collection (ATCC®, LGC Standards s.a.r.l., France). Murine cell lines were purchased from European Collection of Authenticated Cell Culture (ECACC, Sigma-Aldrich). E0771-AKA-Luc2

cells were kindly provided by prof. Massimiliano Mazzone. Following cell lines were used and RRID; year of acquisition are mentioned between brackets; A-172 (CVCL_00131; 2020), A2058 (CVCL_01059; 2020), A2780 (CVCL_0134; 2020), A2780 CpR (CVCL_H745; 2020), A549 (CVCL_0023; 2020), H9C2 (CVCL_0286; 2015), E0771 (CVCL_GR23; 2013), HC-11 (CVCL_0288; 2013), HCT-116 (CVCL_0291; 2019), HME-1 (CVCL_3383; 2015/2020), HUVEC (CVCL_2959; 2015), LS 174T (CVCL_1384; 2015), MDA-MB-231 (CVCL_0062; 2015), MDA-MB-468 (CVCL_0419; 2015), MIA PaCa-2 (CVCL_0428; 2019), NCI-1299 (CVCL_0060; 2020), NCI-292 (CVCL_0455; 2019), PANC-1 (CVCL_0480; 2019) and U-87 MG (CVCL_0022; 2020). Upon arrival, cells were expanded and aliquots were frozen at low passage number to limit deviation from their original identity, as authenticated by the source via STR profiling and CO1 assay. Cells were cultured according to manufacturer's recommendations and propagated at 37°C, 5% CO₂. Experiments were performed within 10 weeks after defrosting at consistent passage number (<20). Mycoplasma testing was performed routinely using the MycoAlert PLUS mycoplasma detection kit (LT07-705, Lonza). Cell lines used for *in vivo* studies were screened for rodent pathogens (IMPACTTM Mouse I package, IDEXX BioAnalytics, Germany).

THOP1 ELISA

Cellular or extracellular/secreted protein levels of THOP1 were determined on total protein extracts and conditioned media (20x concentrated) respectively, using The RayBio® Human Thimet Oligopeptidase ELISA kit (ELH-THOP1, Raybiotech, Georgia, USA). To concentrate secreted proteins in cell-conditioned media, serumfree medium was collected after being conditioned overnight and concentrated using Amicon® ultra-15 Centrifugal Filter Units with 50 kDa cut-off (30 min, 4.000x g, 4°C). Following centrifugation, supernatant was diluted to reach a final concentration factor of 20 (starting volume/assay volume) and was analyzed for THOP1 protein levels. In parallel, cells were placed on ice and intracellular proteins were extracted in RIPA buffer with Pierce protease and phosphatase inhibitor cocktail (Thermo fisher Scientific, Massachusetts, USA). Ten µg total proteins was used for quantification of cellular THOP1 protein expression.

Peptidase activity assay

THOP1 activity in conditioned media was assessed using a custom fluorogenic substrate resembling PhAc-ALGP-Dox (Pepscan B.V., The Netherlands). ALGP was used to couple quencher (2,4-dinitrophenol) and fluorophore β -(7-methoxy-coumarin-4-yl)-Ala-OH, generating a specific substrate that only yields signal after cleavage of the tetra-sequence. Medium from either normal (HME-1) or tumor cells (LS 174 T) was conditioned overnight at 37°C, 5% CO₂. Next, the substrate (10 μ M) was dissolved in conditioned medium and fluorescence was monitored every 15 mins for 6 hrs (Ex 325 nm/Em 392 nm). Relative Fluorescence Units (RFU) were obtained from duplicate wells after background subtraction. THOP1 activity in tumor conditioned media was blocked by preincubation with JMV-390 (10 μ M) for 15 min.

In vitro 2D cytotoxicity and selectivity

Cells were seeded in 96-well plates at optimal cell densities (ranging from 7 - 15 x10³ cells/well). After overnight attachment, cells were exposed to a serial dilution of PhAc-ALGP-Dox decreasing from 100 μ M in 1:3 increments. Dox was used as a reference compound, at concentration 10 times lower. After 72 hrs, cells were rinsed and RPMI-1640 phenol red-free medium containing WST-1 reagent (Roche) was added to assess cell. Absolute cytotoxicity was calculated based on viability normalized to non-treated conditions. Absolute IC₅₀ (IC₅₀) is the concentration required to reduce cell viability with 50%. Relative IC₅₀ (rIC₅₀) is the concentration required to reach 50% of the maximal effect. Maximal toxicity was calculated based on potency at highest concentration tested.

To define safety towards tumor cells, a selectivity index (SI) was defined as the ratio of absolute IC₅₀ in normal (HME-1) versus tumor cells (8).

$$\text{Selectivity Index (SI)} = \frac{\text{Normal cell IC}_{50}}{\text{Cancer cell IC}_{50}}$$

Triplicate values were plotted as mean $\pm$ S.E.M. and each experiment was repeated 3-5 times. GraphPad Prism 7.0 (RRID:SCR_002798) was used for non-linear fitting according to the sigmoidal-4PL model. Outliers were automatically excluded and Log(IC₅₀) values were extrapolated. Similarly, rIC₅₀ and maximal toxicity (100% viability – lowest viability) were deducted from the non-linear regression.

In vitro 3D cytotoxicity

Cells, magnetized with NanoShuttle™-PL (Greiner Bio-One), were seeded in 96-well ULA plates at 5×10^3 cells/well and spheroids were allowed to form for 72 hrs (37 °C, 5% CO₂). For MDA-MB-231 spheroids, addition of 2.5% Matrigel at day 1 was required to drive condensation. To prevent aspiration or disturbance of the spheroids, a magnetic spheroid drive (Greiner Bio-One) was used during manipulation. Next, spheroids were stimulated with different concentrations of Dox or PhAc-ALGP-Dox for 72 hrs. Every 3 to 4 days, culture medium was refreshed. Brightfield microscopy images were taken to calculate spheroid volume using the following formula;

$$V = \pi * \frac{4}{3} * \left(\sqrt{A/\pi} \right)^3$$

where A = area (Fiji ImageJ 2.1.0/1.53 RRID:SCR_003070). Spheroids with a volume exceeding the field of view, were not further quantified (= cut-off). In order to visualize growth over time, sizes were normalized to their respective volume at 72 hrs in culture (pre-treatment).

Tissue distribution and pharmacokinetics

Levels of PhAc-ALGP-Dox or Dox in mouse tissues after IV administration at 92 µmol/kg in tumor bearing mice were determined by LC-MS/MS (Acquity I-Class - Xevo TQS micro, Waters Corporation). Potential intermediates (ALGP-Dox, LGP-Dox, GP-Dox, P-Dox) and Doxorubicinol were similarly monitored. Briefly, tissue homogenate was transferred in a microtube containing the same volume of an AgNO₃ solution (66% w/v) (second dilution factor=2) and extracted with ice-cold Acetonitrile/Methanol (50:50) containing 1 µM internal standard (Doxorubicin ¹³C D₃, dilution factor = 5). After centrifugation, supernatant was transferred to matrix tubes for LC-MS/MS analysis as described above. LOD and LLOQ were respectively 0.076 µg/g and 0.26 µg/g of tissue for PhAc-ALGP-Dox, 0.0066 µg/g and 0.022 µg/g for ALGP-Dox, 0.0061 µg/g and 0.020 µg/g for LGP-Dox, 0.0052 µg/g and 0.017 µg/g for GP-Dox, 0.0048µg/g and 0.016µg/g for P-Dox, 0.0081µg/g and 0.027µg/g for Dox and 0.0041µg/g and 0.014µg/g for Doxorubicinol. Bioanalytical analyses were performed at Laboratoire Chimie Générale, Faculté des Sciences Pharmaceutiques et Biologiques (Lille, France).

In vivo hematotoxicity

As described by Till and McCulloch (9), sublethally irradiated C57BL6 mice (9.5 Gy) were intravenously injected with 1×10^7 hematopoietic stem cells, extracted from the bone marrow of donor mice treated with 1026 mg/kg PhAc-ALGP-Dox or 58 mg/kg Dox. Treatment was performed by means of osmotic minipumps (Alzet 1007D) implanted intraperitoneally. Blood count on donor mice was performed using Abbott Cell-Dyn 3700 hematology analyzer, while in depth characterization of subpopulations was performed via FACS analysis (B cells = $CD45R^+$; CTL = $CD3^+ CD8a^+$; $CD4^+ = CD3^+ CD4^+$; NK = $NK1.1^+$).

In vivo efficacy studies

Studies were conducted in 6- to 8-week-old nu/nu NMRI or C57BL6 female mice (Janvier Laboratories). For orthotopic models, 1×10^6 E0771 cells (50 μ l PBS) were injected into the mammary fat pad of syngeneic C57BL6 mice. For subcutaneous models, single-cell suspensions of 5×10^6 MDA-MB-231 or MDA-MB-468 cells (200 μ l PBS:Matrigel, 1:1) were injected subcutaneously into the right posterior flank. Similarly, 5×10^6 U-87 MG (200 μ l PBS:Matrigel, 1:1), 3×10^6 A2780 CpR, 5×10^6 A549, 5×10^6 NCI-H292, 1×10^7 HCT-116 (200 μ l PBS) were injected subcutaneously into the right posterior flank of NMRI nude mice.

Tumor size was measured every 2 days using a caliper and volume was estimated using $V = 4/3\pi \times (d/2)^2 \times D/2$, where d indicates minor and D major tumor axis. Tumor growth inhibition (TGI%) was calculated as follows: $\%TGI = (1 - [Tt/T0 / Ct/C0] / 1 - [C0/Ct]) \times 100$ where Tt and T0 are the individual volume of treated animal X at time t and 0 respectively, Ct and C0 are mean volume of control group at time t and 0 respectively.

E0771 lung metastatic nodules were contrasted after intratracheal injection of 15% India ink and assessed under a stereomicroscope. MDA-MB-468 lung metastasis was quantified by qPCR measuring the ratio between the human GAPDH expression over murine ribosomal subunit 18s.

PDX models: establishment and maintenance

PDX models were established and maintained via bilateral subcutaneous transplantation of fresh human tumor fragment into the flank of 6-7 weeks old female nu/nu NMRI mice (Janvier Laboratories). Animals bearing the original patient tissue were denominated 'passage 0' (p0). In order to maintain PDX models, p0 mice were sacrificed once tumor growth reached a volume of $\sim 200 \text{ mm}^3$. Tumors were collected and cut in smaller

fragments, part of which were immediately re-transplanted to next generation mice (p1, n=2/model). This process was repeated multiple times and tumor tissue of every passage was characterized histologically and immunohistochemically. Models were considered established after stable characteristics for at least two passages.

Study approval

All procedures were conducted in accordance to the ethical standards for experiments on animals established and approved by the Animal Ethics Committee of KU Leuven (ECD numbers: P064/2014, P082/2017 and P102/2019). Xenografting of tumor tissue from consenting patients was approved by the Medical Ethical Committee of UZ Leuven (S53483). Model establishment and subsequent usage for *in vivo* studies was approved by the Ethics Committee for Laboratory Animals of KU Leuven (P175-2015). All experiments with human material were executed in accordance with the Declaration of Helsinki and in accordance with applicable regulatory requirements and written confirmed consent, approved by UZ Leuven Ethics Committee (S60218).

RESULTS

PhAc-ALGP-Dox is sequentially activated via a tumor specific two-step cleavage, initiated by extracellular THOP1 and further processed by FAP α /DPP4

To identify critical enzymes responsible for the dual-step activation of PhAc-ALGP-Dox (**Supplementary Fig. S1A**), the formation of potential intermediates was monitored upon exposure to recombinant human CD10, neurolysin (NLN) or THOP1, 3 related endopeptidases (EC 3.4.24 family) with highly conserved metal-binding motif and substrate similarities (10). Both THOP1 and CD10 were previously suggested to play an important role in the activation of DTS-201 (3). THOP1 demonstrated improved activity towards PhAc-ALGP-Dox compared to DTS-201, resulting rapid decrease of the full-length molecule ($t_{1/2}$ = 82 min) in favor of the predicted intermediate (GP-Dox) while no free Dox was detected (**Fig. 1A and Supplementary Fig. S1B**). Where CD10 effectively activated DTS-201 (**Supplementary Fig. S1C**), neither NLN nor CD10 were involved in PhAc-ALGP-Dox activation ($t_{1/2}$ > 960 min). Indeed, only neglectable amounts of LGP-Dox were detected after exposure to CD10 (2.65% at 16 hrs), while no intermediates were identified in the presence of NLN (**Supplementary Fig. S1D and E**). Similarly, incubation with FAP α or DPP4 alone did not generate free Dox or any intermediate, confirming the protective role of the capping group against exopeptidase activity (**Supplementary Fig. S1F and G**).

Next, in the presence of THOP1, both FAP α and DPP4 were able to complete the second step and finalize prodrug activation. While GP-Dox is being generated by THOP1 activity and peaks after 4 hrs incubation, free Dox is produced simultaneously from this intermediate in the presence of either DPP4 or FAP α with similar efficiency (57% and 49% conversion at 16 hrs respectively, **Fig. 1B-C**).

To better reflect clinical applicability, RNA expression of PhAc-ALGP-Dox processing enzymes was assessed in biopsies of patient diagnosed with stage IV TNBC. Both THOP1 and FAP α were significantly upregulated compared to normal adjacent tissue (NAT), but not in whole blood from the same patients, excluding the risk of ectopic activation (**Supplementary Fig. S1H-K**).

PhAc-ALGP-Dox activation is sequential and spatially controlled

To demonstrate that sequential activation of PhAc-ALGP-Dox by tumor enriched peptidases is controlled both temporally and spatially, enzymatic activity towards ALGP and subsequent cellular localization of Dox was monitored. First, results from parallel artificial membrane permeability assay indicate that PhAc-ALGP-Dox is cell impermeable ($P_{eff} < 0.017$ nm/s). It is only after cleavage by THOP1 that GP-Dox diffuses into the cell. This biologically inactive intermediate is then cleaved intracellularly by FAP α and/or DPP4, generating active Dox. To validate this principle, normal cells that are not responsive towards the prodrug (HUVECs), were exposed to 20 μ M PhAc-ALGP-Dox for 5 hrs and autofluorescence of Dox was monitored. While no intracellular signal was observed in the absence of recombinant enzymes, administration of THOP1 increased intracellular localization, signifying the requirement of extracellular THOP1 activity for entering the cell. Subsequently, Dox autofluorescence was significantly confined to the nucleus as soon as FAP α was added in addition to THOP1, while blocking FAP α /DPP4 activity prevented nuclear localisation (**Fig. 1D-L**).

To correlate our findings to the tumor-targeting mode of action of PhAc-ALGP-Dox, THOP1 protein levels in tumor cells were compared to normal epithelial cells (HME-1). Quantification reveals a modest increase in intracellular protein expression in MDA-MB-231 and LS 174T compared to normal cells (1.6 and 4.3-fold respectively), but significantly higher abundance in conditioned media (14.2 and 34.3-fold increase (**Fig. 1M**)). Finally, using a mimetic of PhAc-ALGP-Dox, featuring a quencher and fluorophore separated by ALGP, only tumor-conditioned medium effectively activates the substrate, while blocking THOP1 abrogated cleavage (**Fig. 1N and O**).

PhAc-ALGP-Dox is a highly selective drug-conjugate with promising anti-cancer efficacy

To define potency in clinically relevant indications, cell viability was assessed in murine (E0771) and human (MDA-MB-231 and MDA-MB-468) models for TNBC and colon adenocarcinoma (LS 174T). Consistent with the dual-step activation of PhAc-ALGP-Dox, potency was shifted from the parental compound, both in E0771 ($IC_{50} = 0.35$ μ M vs 0.02 μ M) and human cancer cell lines (MDA-MB-231; $IC_{50} = 14.89$ μ M vs 0.31 μ M, MDA-MB-468; 2.07 μ M vs 0.11 μ M and LS 174T; 0.31 μ M vs 0.02 μ M). When compared to DTS-201 however, potency of PhAc-ALGP-Dox was superior in all models (**Supplementary Fig. S2A and B**). Moreover, selectivity of PhAc-ALGP-Dox towards tumor cells was significantly

higher, both in murine and human cell lines (**Fig. 2 and Supplementary Fig. S2C**). Selectivity index, defined as the ratio of IC₅₀ in normal versus tumor cells, was 9- to 129-fold higher than Dox and even 6- to 46-fold superior to DTS-201 (**Supplementary Table S1**). In line with enhanced selectivity, improved safety of PhAc-ALGP-Dox was further highlighted by reduced maximal toxicity in normal compared to tumor cells (**Fig. 2A-E**). To assess the broader applicability, additional cell lines spanning 8 different cancer indications were tested. After validation of abundant THOP1 expression, 14/15 investigated cell lines were effectively targeted by PhAc-ALGP-Dox. Potency (IC₅₀) ranged from 311 nM to 34.25 μ M, whereas HME-1 cells confirmed to be resilient (IC₅₀ > 100 μ M, **Supplementary Table S1**).

While 2D monolayers are relevant for screening purposes, they poorly resemble tumor complexity, with significant differences in drug exposure, cellular organization, growth kinetics and gene expression (11). Especially when considering peptidase-activated prodrugs such as PhAc-ALGP-Dox, results are worthwhile confirming in 3D-spheroids in order to better anticipate *in vivo* response. Exposing MDA-MB-231 spheroids to PhAc-ALGP-Dox dose-dependently reduced spheroid growth (**Fig. 2F-H**). These findings were confirmed using LS 174T spheroids, with equipotent concentrations being approximately 10-fold higher compared to free Dox (**Fig. 2I-K**). Together, these data highlight the potential of PhAc-ALGP-Dox to target tumor cells in a 3D architecture.

Proof-of-Concept: PhAc-ALGP-Dox activation by peptidases in vitro

To confirm the dual-step activation in a cellular context, two elegant approaches were applied. First, the tumor microenvironment was mimicked by exposing normal HME-1 cells to excess recombinant peptidases (gain-of-function). Alternatively, endogenous expression was inhibited in tumor cells (loss-of-function). In line with the *in vitro* kinetics (**Fig. 1**), PhAc-ALGP-Dox cytotoxicity improved in the presence of excess THOP1, resulting in a significant shift of IC₅₀ from ~373.3 μ M to 2.06 μ M (**Supplementary Fig. S2D**). Exogenous presence of FAP α or DPP4 on the other hand, had no noteworthy effect (**Supplementary Fig. S2E and F**). Similarly, exposure of tumor cells to a dose titration of PhAc-ALGP-Dox in the presence of exogenous THOP1, but not FAP α or DPP4 shifted the cytotoxicity near the response towards Dox, while blocking endogenous THOP1 or FAP α /DPP4 activity protected against PhAc-ALGP-Dox cytotoxicity (**Supplementary Fig. S2G-R**). Additionally, enhanced activity of THOP1 towards PhAc-ALGP-Dox compared to DTS-201 was confirmed using a

knock-down approach and a second, more selective THOP1 inhibitor, Cpp-AAF-pAb. Due to the limited window of effective knock-down and short stability of the inhibitor respectively, drug exposure was limited to 16 hrs and cell viability assessed 72 hrs later. Where ~50-70% reduction in THOP1 protein revealed a modest effect on PhAc-ALGP-Dox activation, the specific inhibition with Cpp-AAF-pAb confirmed the greater THOP1-dependency of PhAc-ALGP-Dox compared to DTS-201 in both cell lines investigated (**Supplementary Fig. S3**).

Tissue distribution and pharmacokinetics

Pharmacokinetic properties were evaluated after intravenous injection in healthy mice. PhAc-ALGP-Dox, as well as the free Dox derived from PhAc-ALGP-Dox, show favorable linearity within the dose range investigated (**Supplementary Fig. S4**). At the highest concentration of 849.5 mg/kg, PhAc-ALGP-Dox rapidly distributed with free Dox, GP-Dox and LGP-Dox being the most abundant metabolites in decreasing order ($t_{1/2}$ = 6.5 - 8.5 min, **Fig. 3A**). Compared to administration of Dox (13.3 mg/kg), exposure to free Dox increased only 1.9-fold, although molar concentration of PhAc-ALGP-Dox was 36-fold higher. When comparing equimolar concentrations, free Dox was 19-fold lower following administration of PhAc-ALGP-Dox compared to Dox (**Fig. 3B**).

In order to determine whether PhAc-ALGP-Dox treatment led to a preferential release of Dox in tumor tissue, E0771 tumor-bearing mice were injected with equimolar concentration of PhAc-ALGP-Dox or Dox (94.4 mg/kg or 53.4 mg/kg respectively) and plasma pharmacokinetic parameters are summarized in **Table 1**. Most abundant metabolite in plasma was GP-Dox, followed by free Dox and LGP-Dox. As observed in healthy animals, free Dox exposure was 15-fold lower when compared to equimolar dosage of Dox, while intra-tumoral concentration was only 2.8-fold lower. In addition to free Dox, the only other metabolite detectable in the tumor, as expected after THOP1 cleavage, was GP-Dox. Taken together, PhAc-ALGP-Dox specifically accumulated in the tumor (C_{max} = 25.2 μ M at 5 min) before efficient metabolization (2.5 μ M after 1 h), while Dox presented slower accumulation in tumor (C_{max} = 21.5 μ M at 4 hrs) and elimination (7.3 μ M at 72 hrs).

In systemic tissues, GP-Dox and free Dox were the major metabolites, generally reaching C_{max} within 5 to 30 min after injection, and interestingly, lowest in heart. Consistent with the expected clearance and metabolization, liver and kidney were most exposed to free Dox. Both intact drug-conjugate and the two metabolites remained highest

in kidney. Of note, direct comparison of DTS-201 and PhAc-ALGP-Dox revealed a safer PK profile of the latter, considering that exposure to free Dox resulting from DTS-201 activation was 2 to 3-fold higher in normal organs (**Table 1**).

Next, MALDI-FTICR imaging was used to give a more general view on tissue biodistribution of PhAc-ALGP-Dox and its metabolites in E0771 tumor-bearing mice. Where administration of Dox (23 mg/kg) dispersed homogenously throughout the body, PhAc-ALGP-Dox (849.5 mg/kg) distributed faster, particularly to excretion and well-perfused organs such as kidney, lung and liver, which could be expected for a stable molecule unable to enter healthy cells. Importantly, activated PhAc-ALGP-Dox accumulated in the tumor within 2 hrs after injection and the presence of free Dox remained stable at least up to 48 hrs. On the contrary, the majority of other organs showed negligible amounts of free Dox with the exception of kidney, where the molecule underwent metabolic and renal elimination. Consequently, free Dox from activated PhAc-ALGP-Dox could be detected, but its presence rapidly decreased over time (**Fig. 3C-D**).

PhAc-ALGP-Dox circumvents systemic toxicity associated with Dox treatment in vitro and in vivo

To address the increased safety of PhAc-ALGP-Dox, acute toxicity was assessed in mice. Median lethal dose (LD₅₀) of PhAc-ALGP-Dox was 780 mg/kg compared to 17 mg/kg for Dox, highlighting improved tolerability and allowing to administer 27 times more payload (780 mg/kg = 459 mg Dox/kg). Next, the effects of PhAc-ALGP-Dox on human hematopoietic progenitor cells and cardiomyocytes were further analyzed. In contrast to significant toxicity of Dox, PhAc-ALGP-Dox exhibits better safety profiles towards total myeloid (IC₅₀ = 0.07 μ M vs 0.01 μ M for Dox) and erythroid derived cells (IC₅₀ = 0.05 μ M vs 0.02 μ M for Dox) (**Fig. 4A and B**). In-depth characterization of different human progenitor-derived colonies confirmed the safer nature of PhAc-ALGP-Dox (**Supplementary Fig. S5A-G**).

To investigate the biological impact of PhAc-ALGP-Dox treatment on bone marrow (BM) long-term repopulation ability, *in vivo* transplantation experiments have been performed. Donor mice were treated continuously for 7 days via osmotic minipumps containing Dox (58 mg/kg/wk) or PhAc-ALGP-Dox (1026 mg/kg/wk) (**Supplementary Fig. S5J**). Two days after treatment, blood samples and bone marrow were collected from donor mice. While no alteration was noticed in neutrophil and monocyte count, whole blood

count revealed a drop in white blood cells both in Dox and PhAc-ALGP-Dox treated animals, mainly attributed to a decrease in lymphocytes (**Fig. 4D-G**). FACS analysis confirmed a reduction in B-cells, while CD4⁺ and NK cells were unaffected. In contrast to Dox, PhAc-ALGP-Dox treated mice had 15% less circulating cytotoxic T lymphocytes (CTLs) (**Supplementary Fig. S5L**). Despite these changes, BM from PhAc-ALGP-Dox, but not from Dox treated donors, maintained high repopulation abilities following transplantation. In fact, 80% of mice receiving BM from PhAc-ALGP-Dox treated donors survived throughout the study (day 41 post transplantation), compared to only 30% of animals receiving BM from Dox-treated mice (**Fig. 4C**). Considering that PhAc-ALGP-Dox donors received 10 times higher Dox-equivalent concentration, these data provide important evidences on reduced hematopoietic cytotoxicity, confirming *in vitro* results.

Additionally, safety of PhAc-ALGP-Dox towards cardiomyocytes was evaluated. In contrast to nanomolar potency of Dox in mitotic and differentiated H9C2 rat cardiomyocytes, mitotic cells were considerably less affected by PhAc-ALGP-Dox while differentiated cardiomyocytes were essentially resilient (**Supplementary Fig. S5H and I**). Clinically more relevant, human iPSCs-derived cardiomyocytes were analyzed for signs of acute or chronic toxicity based on cellular impedance, revealing a notably safer profile for PhAc-ALGP-Dox (**Fig. 4H-M**). While Dox-mediated cardiotoxicity was already evident shortly after exposure and increased to 100% by 72 hrs, PhAc-ALGP-Dox induced alterations only at concentrations exceeding equipotency of Dox in cancer cells (>5 μ M) and were delayed in time and reduced in effect size. Similarly, changes in contractility were only observed following exposure to high concentrations of PhAc-ALGP-Dox. Moreover, maximal toxicity did not further increase with higher concentrations and tended to reach a plateau, highlighting the lack of cumulative toxicity. Finally, Dox induced significant arrhythmia, signified by an initial incline of beating rate, rapidly followed by cardiac arrest. Although PhAc-ALGP-Dox triggered increased beating rates at higher concentrations, these effects were reversible and normalized within 72 hrs. Taken together, these results emphasize the significantly improved safety of PhAc-ALGP-Dox.

Finally, to define the most appropriate PhAc-ALGP-Dox dose and regimen for preclinical efficacy studies, MTD was calculated (**Fig. 4N-Q**). Increasing concentrations of PhAc-ALGP-Dox (103, 206 and 309 mg/kg) were dosed weekly in healthy or MDA-MB-468

tumor bearing mice. Confirming the hypothesis that tumors sequester PhAc-ALGP-Dox and reduce systemic exposure, toxicity (when observed) tended to be more severe and mortality was higher in healthy compared to tumor bearing mice. Focusing on tumor bearing mice, 4 cycles of 206 mg/kg PhAc-ALGP-Dox revealed mild but reversible body weight loss (15%) and a temporary decrease of lymphocyte and neutrophil count, while tumor growth inhibition (TGI) was approximately 140%. Based on these results, the highest tolerated dose of a PhAc-ALGP-Dox was defined at 154 mg/kg (QWx4), corresponding to 87 mg/kg Dox equivalent.

PhAc-ALGP-Dox shows evidence of superior efficacy in clinically relevant Xenograft and PDX models.

Efficacy of PhAc-ALGP-Dox was compared to Dox in several tumor models of murine and human origin, including TNBC and STS. Both in a syngeneic orthotopic model (E0771) and a human xenograft model (MDA-MB-231) for TNBC, PhAc-ALGP-Dox significantly improved the therapeutic index of Dox, following superior tolerability while maintaining equipotency in terms of TGI and metastatic dissemination. Histological characterization revealed that PhAc-ALGP-Dox significantly reduced tumor necrosis (**Fig. 5A-F and Supplementary Fig. S6A-B**). Interestingly, mice treated with equimolar concentrations of DTS-201 (155 mg/kg) displayed signs of toxicity, while well-tolerated concentrations resulted in suboptimal efficacy (**Supplementary Fig. S6C**). These data highlight the increased therapeutic index of PhAc-ALGP-Dox compared to equimolar concentrations of DTS-201 or equipotent concentrations of Dox and revealed consistent reduction of tumor necrosis.

Next, the MDA-MB-231 xenograft model was used to investigate whether optimizing route of administration increased efficacy of PhAc-ALGP-Dox. Continuous delivery of PhAc-ALGP-Dox via osmotic minipumps decreased tumor volume in a dose-dependent manner (**Fig. 5G**). At 1026 mg/kg, PhAc-ALGP-Dox treatment stabilized tumor growth with a TGI of 98%, whereas in Dox treated animals TGI did not exceed 84%. Mild, but reversible, body weight loss was observed after administration of Dox, as well as with the highest dose of PhAc-ALGP-Dox (1026 mg/kg) (**Supplementary Fig. S6D**). Importantly, where Dox therapy failed to prevent necrosis, PhAc-ALGP-Dox significantly reduced tumor necrosis at therapeutic concentrations (**Fig. 5H**). These results were confirmed using a second model for TNBC (MDA-MB-468) where PhAc-ALGP-Dox treatment not only induced important

inhibition of tumor growth, but also reduced metastatic dissemination (**Fig. 5I and J**). Moreover, therapeutic concentrations of PhAc-ALGP-Dox resulted in superior TGI compared to Dox (151% vs 70%). Again, reduction of tumor volume corresponds to a significant decrease in necrosis following treatment with 1026 mg/kg/wk PhAc-ALGP-Dox, without changes in body weight (**Fig. 5K and Supplementary Fig. S6E**).

The potential of PhAc-ALGP-Dox in targeting metastatic cells *in vivo* was evaluated in a model for experimental lung metastasis. E0771-AKA-Luc2 cells were injected into the lateral tail vein in order to mimic metastatic homing and growth into the lung. Mice receiving PhAc-ALGP-Dox treatment, exhibited significantly lower metastatic burden without signs of toxicity, resulting in clear improvements of overall survival (**Fig. 5L and M and Supplementary Fig. S6F-H**). To emphasize the broad applicability of PhAc-ALGP-Dox, efficacy was demonstrated in numerous additional human xenograft models, including colorectal cancer, glioblastoma, non-small cell lung cancer (NSCLC) and cisplatin resistant ovarian cancer. A summary is shown in (**Supplementary Table S1**). Recently, patient-derived xenografts (PDX) are favored over cell-line derived xenografts, as they better reflect the heterogeneity and properties of the original tumor. Therefore, PhAc-ALGP-Dox efficacy was confirmed using two PDX models of leiomyosarcoma. In both models, TGI following PhAc-ALGP-Dox treatment was superior when compared to Dox (**Fig. 5N and O**).

Altogether, these preclinical results emphasize improved safety of PhAc-ALGP-Dox and potential superiority compared to Dox at well-tolerated concentrations, leading to an increased therapeutic index and promising clinical applicability.

DISCUSSION

Although Dox remains a cornerstone of many anticancer therapies, its potential remains limited by cumulative toxicities, despite various attempts to improve the therapeutic index. In this study, PhAc-ALGP-Dox has proven to be a valid alternative with broad applicability, favorable tissue distribution and improved therapeutic index due to its tumor-targeting nature. The unique mode of activation is mediated by a sequential and spatially controlled activation. Where DTS-201 activation is suggested to be mediated by both THOP1 and CD10 (2,3), PhAc-ALGP-Dox cleavage is more effectively and more exclusively driven by THOP1. Indeed, similar oligopeptidases, such as CD10 and NLN, or

more general matrix-metalloproteases involved in tumor biology (e.g. MMP2 and MMP9), were excluded as potential activators of PhAc-ALGP-Dox. Intriguingly, the expression of THOP1 is upregulated in many tumor types and has been repeatedly correlated with prognosis (12-16). On the other hand, expression of CD10 is less tumor specific and, although indisputable, its role in cancer remains controversial (17). In addition, hematopoietic cells rely on CD10 for differentiation and maturation (18,19), increasing the risk of DTS-201 related myelosuppression, the main toxicity observed in a Phase I clinical trial (6). Although the presence of THOP1 in normal tissues has been described, detection is confined to the intracellular space (20), while extracellular THOP1 activity is considerably more restricted to the tumor microenvironment. Indeed, we demonstrated that PhAc-ALGP-Dox is cell impermeable before being activated by extracellular THOP1 (**Fig. 1**). Moreover, tumor specificity could be twofold, since not only THOP1 expression is upregulated, but also pathways responsible for its secretion are more active in cancer cells (21-26). THOP1 secretion occurs via the non-canonical pathway and is enhanced following protein kinase A (PKA) mediated phosphorylation and association with 14-3-3 ϵ (27-30). The role of PKA and 14-3-3 ϵ in tumor progression, vascularization and metastasis has been well described (14,26,31,32), and could increase the pool of extracellular THOP1 during progression. Moreover, activated immune cells could also contribute and sustain THOP1 within the tumor microenvironment (12,33), maintaining PhAc-ALGP-Dox activation. Altogether, these factors mediate tumor specific activation of PhAc-ALGP-Dox to a cell permeable intermediate, which rapidly enters tumor cells where it is further processed to active Dox in a self-sustainable way, limiting the chance of enzyme exhaustion and subsequent resistance.

The importance of activating enzymes was further demonstrated by blocking endogenous enzymes in tumor cell cultures. Inhibiting the activity of either THOP1 or FAP α /DPP4 abrogated PhAc-ALGP-Dox cytotoxicity, while ~50-70% reduction in THOP1 protein expression provided a modest but apparent shift in potency (**Supplementary Fig. 2 and 3**). Indeed, the residual THOP1 could still be responsible for activating PhAc-ALGP-Dox and causing cytotoxicity. However, and in line with higher THOP1-dependency, the effects on cytotoxicity following either limited knockdown or specific THOP1 inhibition were more pronounced for PhAc-ALGP-Dox as compared to DTS-201. Furthermore, mimicking the tumor secretome in normal cell cultures by adding exogenous recombinant enzymes

resulted in activation of PhAc-ALGP-Dox. Similarly, enriching the extracellular presence of THOP1 in tumor cells increased the potency to a similar level as Dox alone, signifying complete activation (**Supplementary Fig. 2**). Since the unique mode of activation hijacks pathways used by tumor cells to progress, PhAc-ALGP-Dox is applicable to a broad variety of solid tumors as demonstrated by *in vitro* potency and *in vivo* efficacy in several preclinical models (**Supplementary Table 1**). Somewhat intriguing, the mere expression of THOP1 was required, but not sufficient, to predict *in vivo* response. Indeed, while all THOP1-expressing models were responsive to PhAc-ALGP-Dox, potency nor efficacy correlates with THOP1 expression *per se*, although a positive trend towards maximal efficacy could be observed *in vitro*. Most likely, increased expression in tumor cells, combined with the significantly higher extracellular activity underlies the rapid activation and targeted delivery of large quantities of payload. This concept was further highlighted by the favorable tissue distribution of PhAc-ALGP-Dox (**Fig. 3**). Although one could argue that introduction of a linear peptide moiety favors renal clearance, we demonstrated that, despite the short half-life of PhAc-ALGP-Dox, large quantities of active payload are delivered specifically to the tumor site. Tumor requisitioning of PhAc-ALGP-Dox was further highlighted by the differential MTD in healthy versus tumor bearing mice, where systemic exposure was potentially reduced due to sequestration within the tumor (**Fig. 4M-P**). Consistent with the expected metabolism and clearance, intact prodrug and metabolites were detected in kidney and to a lesser extent in liver. However, passage was transient without significant conversion to Dox, and therefore expected to be cleared. Indeed, no signs of nephrotoxicity were observed. Extra attention was given to the heart, since cardiotoxicity is a major concern for Dox-based therapies. Encouragingly, neither Dox nor its toxic metabolite, doxorubicinol, were detected following PhAc-ALGP-Dox administration. Improved safety towards cardiomyocytes was further demonstrated in hiPSC-CMs, where changes in cellular impedance, contractility or beating rate were only observed at concentrations exceeding equipotency in tumor cells. Even at supraphysiological concentrations, alterations in cardiac function were delayed in time, less pronounced as compared to Dox and reversible (**Fig. 4G-L**). Similarly, in-depth analysis of hematotoxicity, the second common dose-limiting toxicity of Dox, revealed transient effects of PhAc-ALGP-Dox on blood parameters with a significant drop in lymphocytes, similar to what was reported for Dox (34-36). However, survival was significantly improved when using bone marrow explants from treated donors to repopulate

sublethally irradiated recipient mice. This indicates that, in contrast to Dox, the reduction in blood cells following PhAc-ALGP-Dox treatment is reversible without underlying toxicity on hematopoietic progenitor cells.

Despite its limitations, anthracyclines remain one of the most used drug classes in clinic to treat breast cancer with an ORR of 30-50%. However, their use in metastatic setting is often limited due to concerns that cumulation from adjuvant chemotherapy raises the risk of cardiotoxicity (37). The favorable profile of PhAc-ALGP-Dox leads to improved inhibition of primary tumor growth in multiple models, secondary to high tumor retention of activated Dox (**Fig. 3, 5 and Supplementary Table 1**). This resulted in decreased tumor necrosis when compared to Dox treatment, indicating a possible switch from the canonical pro-apoptotic pathway, to a “softer” antiproliferative and death-inducing signal cascade. This phenotype is currently under investigation and reveals similarities to mitotic catastrophe.

In addition to effectively targeting the primary tumor in a variety of models, these results also indicate a suppressive effect on metastatic dissemination in a xenograft model for breast cancer (**Fig. 5B**). However, the intrinsic limitation of preclinical models does not allow to discriminate between a direct impact of PhAc-ALGP-Dox on metastatic behavior or simply a consequence to significant primary tumor growth inhibition following the treatment. Using a murine model for experimental lung metastasis, the direct effect of PhAc-ALGP-Dox on metastatic growth was demonstrated to be superior to Dox. Although metastatic cells are difficult to target, their pro-metastatic properties also render them more susceptible to PhAc-ALGP-Dox treatment. Mechanisms used by cancer cells to detach from the primary lesion, survive in circulation and colonize distant sites are far from elucidated, but include proteolytic activity during multiple stages of metastatic dissemination (38-40). While the role of zinc(II)-dependent endopeptidases herein has been well-studied (41,42), the specific contribution of THOP1 to distant colonization is less understood. Nevertheless, it is expected that secretory pathways are significantly upregulated in metastatic cells in order to orchestrate the proteolytic activity required for invasion and colonization. As such, THOP1 secretion is potentially stimulated as well, increasing PhAc-ALGP-Dox activation. Intriguingly, THOP1 expression has been repeatedly linked to metastasis in NSCLC (12), renal clear cell carcinoma (43) and HCC (15). Whether, and how, THOP1 expression correlates to metastasis and disease prognosis remains a

matter of debate and should be further investigated (10). Nevertheless, we have demonstrated that, in addition to efficacy on the primary tumor, PhAc-ALGP-Dox is superior to Dox in targeting metastatic growth.

In a clinical setting, Dox remains the first-line standard-of-care treatment in STS patients with locally or advanced metastasis, despite poor response rates (<15%), underscoring the high medical need (44). The potential of PhAc-ALGP-Dox as a new effective therapy was demonstrated in PDX models derived from patients with grade III leiomyosarcoma. These data corroborate the superior and statistically significant antitumor activity of PhAc-ALGP-Dox as compared to Dox and anticipate the improved therapeutic potential in a larger setting of STS (7,45). While STS could be an interesting indication for clinical development, the extensive applicability of PhAc-ALGP-Dox in a variety of solid tumors was apparent. Compared to other targeted strategies, such as ADCs or PDCs, PhAc-ALGP-Dox is not limited to the presence of specific epitopes in order to be effective. In contrast, it requires an extracellular pool of THOP1 to initiate intracellular entrapment of the payload, which has proven to be highly tumor specific and applicable to a broad range of solid tumors.

Taken together, the unique sequential and spatially controlled two-step activation of PhAc-ALGP-Dox, driven by extracellular THOP1 and cytoplasmic FAP α and/or DPP4 respectively, results in a molecule with superior therapeutic value compared to Dox. In addition to the tumor-favoring biodistribution, these findings show an improved therapeutic index in multiple preclinical models for solid tumors, including TNBC, colorectal cancer, glioblastoma, NSCLC and cisplatin resistant ovarian cancer. Moreover, the superiority compared to Dox was highlighted using clinically relevant PDX models of STS, emphasizing the extensive clinical potential of PhAc-ALGP-Dox.

AUTHOR CONTRIBUTIONS

AC designed, performed and analyzed the *in vivo* data. Similarly, LVH was responsible for the *in vitro* results confined in this publication. AC and LVH wrote the manuscript. BVR performed the *in vivo* experiments on STS PDX, under the supervision of AW and PS, who also revised the manuscript. NDG, MDP and MD were involved in the daily *in vitro* activities, while TJ, MP and MD assisted with *in vivo* studies. CRD performed the bone marrow transplantation under the supervision of MM. OD was responsible for the chemistry, design and synthesis of PhAc-ALGP-Dox. PP, GR and NK were involved in the design of the experiments and edited the manuscript.

ACKNOWLEDGEMENTS

In addition, we would like to express our gratitude to Em. Prof. Dr. Désiré Collen for his comprehensive support for this program. Our appreciation goes out to Dr. Catherine Piveteau from the University of Lille for the services she provided related to mass spectrometry. The authors thank David Bonnel and Mathieu Gaudin at Imabiotech for the results regarding PhAc-ALGP-Dox mass spectrometry imaging and tissue distribution.

In memory of professor André Trouet (1936-2014).

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TABLES

Tissue	Drug	Metabolites	Tumor bearing mice (92 μ mol/kg)					
			$t_{\max}$	$C_{\max}$	AUC	$t_{1/2\alpha}$	$t_{1/2\beta}$	CL
Heart	PhAc-ALGP-	PhAc-ALGP-Dox	5	19	3.7	0.17		
		GP-Dox	5	1.65	2.3	0.3	7	
	Doxorubicin	Dox	30	4.12	94	8.2	28	
		DoxOL		<LoQ				
		Dox	30	115	1933	5.6	34	
	DTS-201*	DoxOL	240	0.86	54	47		
		Succ- β ALAL-	5	35.9	15.1	0.2	0.5	
		Dox	60	10	266	8	39	
		DoxOL		<LoQ				
Kidney	PhAc-ALGP-	PhAc-ALGP-Dox	5	530	388	0.1	9	
		LGP-Dox	5	5.6	3.7	0.1	3.3	
		GP-Dox	5	54	288	0.2	12.7	
	Doxorubicin	Dox	5	80	584	1	16	
		DoxOL	30	1.96	20.8	1	19.7	
		Dox	30	339	6025	2.7	36	
	DTS-201*	DoxOL	30	6.8	168	2.5	49	
		Succ- β ALAL-	15	811	771	0.4	10.7	
		Dox	240	93	1983		17.6	
		DoxOL	240	1.48	49.7		27.1	
Liver	PhAc-ALGP-	PhAc-ALGP-Dox	5	69	152.5	0.7	16.8	
		GP-Dox	5	5.3	72.2	1.4	14.8	
		Dox	30	16	235	2.1	15	
	Doxorubicin	DoxOL	240	0.44	10.6		21.7	
		Dox	5	189	2184	2.1	26	
		DoxOL	1	6	104	2.2	33.3	
	DTS-201*	Succ- β ALAL-	15	49	48	0.6	20.5	
		Dox	60	14	449	25.2		
		DoxOL	120	0.67	30.8		33.4	
		DoxOL	120	0.67	30.8		33.4	
Tumor	PhAc-ALGP-	PhAc-ALGP-Dox	5	25.2	16.9	0.3	2.6	
		GP-Dox	15	20.85	59.6	0.5	10	
		Dox	240	6.72	459		46	
	Doxorubicin	DoxOL		<LoQ				
		Dox	120	21.4	1327		53	
		DoxOL	2880	0.12	8			
	DTS-201*	Succ- β ALAL-	5	56.5	25.6	0.4		
		Dox	720	13.3	988		36	
		DoxOL		<LoQ				
		DoxOL		<LoQ				
Plasma	PhAc-ALGP-	PhAc-ALGP-Dox	5	560	156.5	0.21		
		LGP-Dox	5	0.74	0.133	0.15		
		GP-Dox	5	3.7	1.49	0.2		
	Doxorubicin	Dox	5	1.2	0.74	0.2	9	
		DoxOL		<LoQ				
		Dox	5	7.09	11.3	0.2	13	135
	DTS-201*	DoxOL		<LoQ				
		Succ- β ALAL-	5	243	121.3	0.25		12.6
		Dox	30	0.404	1.41	0.6	16.7	
		DoxOL		<LoQ				

Table 1. Pharmacokinetic properties and tissue distribution of Dox, DTS-201 and PhAc-ALGP-Dox and

intermediates in E0771 tumor bearing mice. *For DTS-201, only the parent molecule and Dox, but no intermediates, were measured.

FIGURE LEGENDS

Fig. 1. PhAc-ALGP-Dox is activated sequentially by extracellular THOP1 and cytoplasmic DPP4/FAP α in the tumor microenvironment. (A-C) Generation of PhAc-ALGP-Dox cleavage products in the presence of recombinant enzymes (THOP1, 0.1 μ g/ml; FAP α , 0.04 μ g/ml or DPP4, 0.04 μ g/ml). Data is represented as mean $\pm$ SD of triplicate analysis, LoQ = 3 nM. **(D)** Quantification of Dox autofluorescence following exposure to 20 μ M PhAc-ALGP-Dox for 5 hrs. Nuclear/cytoplasmic fluorescence was assessed in HUVEC cells in the presence of recombinant THOP1 (0.1 μ g/ml) alone or together with either recombinant FAP α (0.04 μ g/ml) or PT-100 (300 nM), an inhibitor of FAP α /DPP4. Bars represent mean + SD of n=8-12. Asterisks indicate significant differences vs no enzyme or as specified by brackets, ***p<0.001, ****p<0.0001 defined by one-way ANOVA corrected for multiple comparisons (Holm-Sidak). **(E-L)** Representative images of HUVEC cells stimulated with PhAc-ALGP-Dox alone **(E-F)**, together with THOP1 **(G-H)**, THOP1 and FAP α **(I-J)** or THOP1 and PT-100 **(K, L)**. Top panels are merged images of cytoplasmic (Agglutinin, green), nuclear (DAPI, blue) or Dox (autofluorescence, red). Bottom panels are black-white images of Dox autofluorescence. Scale bar = 20 μ m. **(M)** Quantification of ELISA data of human THOP1 protein levels in cell lysates and conditioned media of cancer cells (MDA-MB-231 and LS 174T) compared to normal (HME-1) cells. Bars are mean + SD of 3 independent ELISAs run in duplicate. Asterisks indicate significant differences vs no enzyme or as specified by brackets, ***p<0.001, ****p<0.0001 defined by One-way ANOVA corrected for multiple comparisons (Holm-Sidak). **(N)** Kinetic activation of Dnp(k)-ALGP-CouAla by extracellular peptidases in normal (HME-1, blue) or tumor (LS 174T, purple) conditioned medium. Dashed purple line represents the signal in tumor conditioned media, pre-incubated with a THOP1 inhibitor (THOPi, 10 μ M) **(O)** Quantification of Dnp(k)-ALGP-CouAla conversion after 180 min. Bars are mean + SD, pooled from 3 independent experiments (n=6) **p<0.01 as defined by One-way ANOVA.

Fig. 2. PhAc-ALGP-Dox is highly potent and selective towards in vitro cancer models. (A-E) Dose-response curves after 72 hrs exposure to Dox (blue) or PhAc-ALGP-Dox (purple) in 2D monolayers for **(A)** murine TNBC (E0771), **(B)** normal murine epithelium (HC-11), **(C)** human TNBC (MDA-MB-231 and MDA-MB-468), **(D)** human CrC (LS 174T) or **(E)** normal human epithelium (HME-1). Graphs are presented as sigmoidal non-linear fittings, normalized to non-treated controls. **(F-H)** Growth of MDA-MB-231 spheroids after exposure to different concentrations of **(F)** Dox or **(G)** PhAc-ALGP-Dox. **(H)** Representative bright field images of spheroids at day 17. **(I-K)** Shows the growth of LS 174T spheroids treated with **(I)** Dox or **(J)** PhAc-ALGP-Dox. **(K)** Representative bright field images of LS 174T spheroids at day 14. Data are represented as mean $\pm$ SEM of 3-5 experiments, run in triplicate (n= 9-15). ## $p < 0.01$, **** $p < 0.0001$ vs controls as defined by Two-way ANOVA. Scale bar = 200 μ m. TNBC = triple negative breast cancer, CrC = colorectal carcinoma, NT = non-treated.

Fig. 3. Plasma levels and tissue distribution of PhAc-ALGP-Dox and Dox. (A) Graph showing the plasma levels of PhAc-ALGP-Dox, its potential intermediates and Dox after IV administration of 849.5 mg/kg PhAc-ALGP-Dox in healthy mice (n=5). **(B)** Graph showing the plasma levels of Dox after IV administration of equimolar doses PhAc-ALGP-Dox (23.6 mg/kg) or Dox (13.3 mg/kg) in healthy animals (n=5). **(C)** Tissue imaging by MALDI-FITCR MSI depicting the distribution of Dox in E0771 orthotopically implanted tumor bearing mouse whole body sections at 24h and 48h post IV administration with PhAc-ALGP-Dox (849.5 mg/kg) or Dox (23 mg/kg). **(D):** H&E-staining (left panel) and overlapping imaging by MALDI-FITCR MSI (right panels) depicting the distribution of GP-Dox, Dox and PhAc-ALGP-Dox in E0771 orthotopically implanted tumor sections at 15 min post IV administration with PhAc-ALGP-Dox (849.5 mg/kg).

Fig. 4: PhAc-ALGP-Dox shows reduced hematotoxicity and cardiotoxicity as well as improved MTD with tumor sequestration in tumor bearing mice. (A-B) Dose-response curves for the effect of continuous exposure (14d) to PhAc-ALGP-Dox on Human **(A)** erythroid and **(B)** myeloid progenitor proliferation using MethoCultTM GF H84434. **(C)** Kaplan-Meier plot describing the survival rate of recipient mice after BMT of vehicle, Dox (58 mg/kg/wk) or PhAc-ALGP-Dox (1026 mg/kg/wk) treated donors. Mice were monitored for 41d following BMT (n=6). BMT = bone marrow transplantation. Gehan-Breslow-Wilcoxon test $p=0.03$. **(D-F)** Blood count of donor mice treated with Dox (58 mg/kg/wk) or PhAc-ALGP-Dox (1026 mg/kg/wk) by means of osmotic minipumps; whole blood was analyzed at the time of bone marrow collection. Data represents mean $\pm$ SD (n=8). **** $P<0.0001$ versus control as defined by Two-way ANOVA. **(G-L)** Impedance-based cardiotoxicity of Dox (blue curves) and PhAc-ALGP-Dox (purple curves) in hiPSC-CMs on base impedance, contraction amplitude and beat rate. hiPSC-CMs = human induced pluripotent stem cell derived cardiomyocytes. Data of quadruplicate values is represented as mean $\pm$ SD. **(M-Q)** PhAc-ALGP-Dox dose-response in healthy vs MDA-MB-468 tumor bearing mice. Body weight **(M, O)**, survival rate **(N, P)** and tumor volume **(Q)** were periodically monitored during and after the treatment (as indicated by arrows). Data represents mean $\pm$ SD (n=5). **** $P<0.0001$ versus control (Saline) as defined by Two-way ANOVA; Gehan-Breslow-Wilcoxon test $p<0.0001$ (N) and $p=0.0013$ (P).

Fig. 5. In vivo efficacy of PhAc-ALGP-Dox. (A-D) The graphs show the tumor volume (**A**) and survival rate (**C**) of E0771 TNBC orthografts implanted in C57/Bl6 mice treated with Dox (4.4 mg/kg) or PhAc-ALGP-Dox (154 mg/kg). Mice were treated with IV bolus injection twice a week for a total of 4 cycles as indicated by arrows. The number of lung metastatic nodules of each individual group (**B**) and histological quantification of tumor necrosis in H&E-stained tumor sections (**D**) were determined at the day of sacrifice as indicated in the figure. Data represents average + SD (n=8). *p=0.011; **P<0.01 ****p<0.0001 versus vehicle as defined by One-way (D) or Two-way ANOVA (A); Gehan-Breslow-Wilcoxon test p<0.0001 (C). **(E-H)** The graphs show the tumor volume of MDA-MB-231 TNBC xenografts implanted in NMRI nude mice treated with **(E)** bi-weekly IV bolus infusion of Dox (4.4 and 8.8 mg/kg) or PhAc-ALGP-Dox (63 and 154 mg/kg) for 5 cycles in total or **(G)** by means of osmotic minipumps intraperitoneally implanted delivering 58 mg/kg/wk Dox or 103 or 1026 mg/kg/wk PhAc-ALGP-Dox for one week. At the end of the study, tumor necrosis in IV injected **(F)** and in osmotic minipump treated **(H)** mice was quantified in H&E-stained tumor sections as indicated in the figure. Data represents average + SD (n=8). *p<0.03; ***P<0.0004 ****p<0.0001 versus Control or #p<0.01; ##p<0.001 versus Dox (58mg/kg) as defined by One-way (F, H) or Two-way ANOVA (E, G). **(I-K)** The graph shows the tumor volume **(I)** of MDA-MB-468 TNBC xenografts implanted in NMRI nude mice treated by means of osmotic minipumps intraperitoneally implanted delivering 58 mg/kg/wk Dox or 103 or 1026 mg/kg/wk PhAc-ALGP-Dox for one week. In brackets the number of mice died during the study. At the end of the study, lung metastatic dissemination was determined by qPCR measuring human GAPDH copy number in murine lung tissue **(J)** and tumor necrosis **(K)** was quantified in H&E-stained tumor sections. Data represents average + SD (n=9). *p<0.03; **P=0.006 ***P<0.0009 ****p<0.0001 versus Control or ##p=0.0015 versus Dox (58mg/kg) as defined by One-way (J, K) or Two-way ANOVA (I). **(L, M)** The plot quantifies the relative metastatic growth of E0771 experimental lung colonies **(L)** and survival rate **(M)** treated with corresponding different concentration of Dox, or PhAc-ALGP-Dox as indicated in the figure. Arrows indicate when mice were treated. Data were normalized toward value at day of randomization (d21) to homogenize the variability related to extravasation and lung colonization. Mice received the treatment via TV injection at the time indicated by the arrows. Data represents median of bioluminescence signal (n=9 per group) (*p=0.0179; ****p<0.0001 versus control; ##p=0.0064 versus Dox); Gehan-Breslow-Wilcoxon test

*p=0.0034 (M). (N, O) Tumor volume assessment during treatment of two different models of patient derived leiomyosarcoma xenografted in NMRI nude mice. Data are presented as relative tumor volume (%) compared to the baseline. Mice received the weekly treatment via TV injection at the time indicated by the arrows. In brackets the number of mice died during the study. All data points are shown as mean of relative tumor volume $\pm$ SD (n=10); ***P=0.0002 ****p<0.0001 versus Control or #####p<0.0001 versus Dox (5mg/kg) as defined by Two-way ANOVA.*

Fig. 1

Fig. 3

Fig. 4

Molecular Cancer Therapeutics

PhAc-ALGP-Dox, a novel anti-cancer prodrug with targeted activation and improved therapeutic index

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Mol Cancer Ther Published OnlineFirst February 11, 2022.

Updated version	Access the most recent version of this article at: doi: 10.1158/1535-7163.MCT-21-0518
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